

MODELING AND ANALYSIS OF ADIPOCYTES DYNAMIC WITH A DIFFERENTIATION PROCESS

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Abstract. We propose in this article a model describing the dynamic of a system of adipocytes, structured by their sizes. This model takes into account the differentiation of a population of mesenchymal cells into preadipocytes and of preadipocytes into adipocytes; the differentiation rates depend on the mean adipocyte radius. The considered equations are therefore ordinary differential equations, coupled with an advection equation, the growth rate of which depends on food availability and on the total surface of adipocytes. Since this velocity is discontinuous, we need to introduce a convenient notion of solutions coming from Filippov theory. We are consequently able to determine the stationary solutions of the system, to prove the existence and uniqueness of solutions and to describe the asymptotic behavior of solutions in some simple cases. Finally, the parameters of the model are fitted thanks to some experimental data and numerical simulations are displayed; a spatial extension of the model is studied numerically.

Résumé. Nous proposons dans cet article un modèle décrivant la dynamique d'un ensemble d'adipocytes structurés en taille. Ce modèle tient compte de la différenciation d'une population de cellules mésenchymales en préadipocytes et des préadipocytes en adipocytes; les taux de différenciation dépendent du rayon moyen des adipocytes. Les équations considérées sont, par conséquence, des équations différentielles ordinaires, couplées avec une équation d'advection, dont le taux de croissance dépend de la nourriture disponible et de la surface totale des adipocytes. Comme la vitesse est discontinue, nous introduisons une notion appropriée des solutions, provenant de la théorie de Filippov. Nous sommes alors en mesure de déterminer les solutions stationnaires du système, de prouver l'existence et l'unicité de solutions et de décrire le comportement asymptotique des solutions dans certains cas simples. Finalement, les paramètres du modèles sont estimés grâce à des données expérimentales et des simulations numériques sont présentées; une extension spatiale du modèles est étudiée numériquement.

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1. INTRODUCTION

Obesity is a worldwide major public health issue that doubled since 1980 and affects nowadays almost two billions of adults considered as overweight and 600 millions considered as obese [12]. Strikingly, obesity is the most prevalent cause for the development of cardio-metabolic diseases (cardiovascular diseases, type 2 diabetes, and liver diseases) as well as cancer, increasing mortality and morbidity and justifying the need for intensive research and intervention policy.

Obesity is characterized by an increase in adipose tissue (AT) mass. This expansion of AT is a complex process which requires succeeding steps of proliferation, differentiation and maturation of the cells from the adipocytes lineage [2]. Indeed, within AT, vascular-resident adipose progenitor cells (APCs) proliferate and, under specific signals, differentiate into pre-adipocytes. Pre-adipocytes also expand through proliferation before to differentiate into small mature adipocytes. Mature adipocytes have an impressive capacity of expanding their volume by more than 30-fold through triglyceride accumulation in lipid droplets [7, 16]. Ultimately, one single large lipid droplet occupies most of the cytoplasm and stiffens locally the AT [20]. The mechanical forces generated by hypertrophic stiff adipocytes may both limit their size and stimulate the differentiation of APCs and pre-adipocytes to recruit new adipocytes [15]. Mature adipocyte size is not only critical for adipogenesis initiation but also for adipocyte functions. Indeed, hypertrophic adipocytes have less ability to properly store lipids, resulting in spillover of lipids and excessive fat deposition in other tissues, both favorizing cardio-metabolic diseases. Although there is growing evidence that impaired AT expandability plays a pivotal role in obesity-related cardio-metabolic diseases, the molecular and cellular basis of this phenomenon is complex and far from being understood. Indeed, the expansion of AT depends on a large number of parameters including the rate of APCs and pre-adipocytes proliferation/differentiation/death, the mechanical feedback loop of adipogenesis stimulation, the size of the adipocytes and the kinetic of their death.

The pathological implication of these phenomena is a motivation for developing new approaches for a better understanding of the AT formation. Mathematical modeling can provide useful insights, in particular for identifying leading parameters. Noticeably, the mechanical feedback loop of adipogenesis stimulation is certainly a pivotal parameter that could control the ability of adipose tissue to expand through the recruitment of new adipocytes. We refer the reader to [17, 18] for attempts in this direction. Here, we shall present a different modeling of the AT development, including some differentiation processes and a velocity growth depending on the total surface, and investigate, theoretically and numerically, the main features of the adopted model.

1.1. Description of the homogeneous in space model

We think of the process as a compartment model with three populations of cells: mesenchymal, pre-adipocytes and adipocytes, the latter population being structured by the size of the cells. Let $t \mapsto m(t)$ and $t \mapsto p(t)$ stand for the number of mesenchymal, and pre-adipocytes, respectively; in the first five sections, both quantities depend only on the time variable $t \geq 0$. Adipocytes are described by their radius distribution function $(t, r) \mapsto a(t, r)$: for given $0 \leq r_1 \leq r_2$, the integral $\int_{r_1}^{r_2} a(t, s) ds$ gives the number of adipocytes with a radius r between r_1 and r_2 , at time $t \geq 0$.

Mesenchymal and pre-adipocytes undergo proliferation and mortality. Furthermore, mesenchymal cells differentiate into pre-adipocytes, while pre-adipocytes differentiate into adipocytes. The mutation of pre-adipocytes gives rise to adipocytes with radius $r_* \geq 0$, and r_* will be the minimal radius within the adipocytes population. Adipocytes can undergo mortality and dynamic change of their radius. Radius changes are modeled with a growth rate function $(t, r) \mapsto V(t, r)$. The expression of the growth rate function V will be determined later on, through volume considerations. As it will be detailed below, we assume the existence of a critical size $r_c > 0$, which stands for the maximal value of adipocyte radius.

The unknowns depend on the time variable $t \in [0, +\infty)$ and, for the adipocyte distribution, on the radius variable $r \in [r_*, +\infty)$. The evolution of the population of mesenchymal cells, pre-adipocytes and adipocytes is

governed by the following set of equations, defined on the domain $(t, r) \in [0, +\infty) \times [r_*, +\infty)$

$$\begin{cases} \frac{dm}{dt}(t) = -\gamma m(t) + \alpha m(t) - \beta(\bar{r}(t))m(t), \\ \frac{dp}{dt}(t) = -\gamma' p(t) + \alpha' p(t) - \beta'(\bar{r}(t))p(t) + \beta(\bar{r}(t))m(t), \\ \frac{\partial a}{\partial t}(t, r) + \partial_r (Va)(t, r) = -\gamma'' a(t, r), \end{cases}$$

where all the parameters of the model are nonnegative and can be collected as follows:

- α, α' proliferation rates for m and p ,
- β, β' differentiation rates for m and p , which depend on the mean radius of adipocytes $\bar{r}(t)$ at time t ,
- $\gamma, \gamma', \gamma''$ mortality rates for m, p and a ,
- r_m radius of mesenchymal cells,
- r_* emergence radius of adipocytes (minimal radius) and radius of pre-adipocytes,
- r_c maximal radius of adipocytes,
- $V(t, r)$ growth rate of an adipocyte of radius r at time t .

Denoting by $\delta = \alpha - \gamma$ and $\delta' = \alpha' - \gamma'$, we obtain the following system:

$$\frac{dm}{dt}(t) = \delta m(t) - \beta(\bar{r}(t))m(t), \quad (1a)$$

$$\frac{dp}{dt}(t) = \delta' p(t) - \beta'(\bar{r}(t))p(t) + \beta(\bar{r}(t))m(t), \quad (1b)$$

$$\frac{\partial a}{\partial t}(t, r) + \partial_r (Va)(t, r) = -\gamma'' a(t, r). \quad (1c)$$

Initial data and boundary conditions. The system is complemented by initial data

$$m(0) = m_0 \geq 0, \quad p(0) = p_0 \geq 0, \quad (2a)$$

$$a(0, r) = a_0(r) \geq 0. \quad (2b)$$

Since $V(t, r_*)$ is positive, we also need to prescribe the boundary condition for a when $r = r_*$; this is where we take into account the differentiation of the pre-adipocytes into adipocytes:

$$V(t, r_*) a(t, r_*) = \beta'(\bar{r}(t)) p(t). \quad (3)$$

For the largest adipocytes, the growth rate vanishes (see below), and we simply assume that $V(t, r) a(t, r) = 0$ for $r > r_c$. It means that adipocytes beyond a certain size do not exist. Consistently, we also assume that the support of a_0 is included in $[r_*, r_c]$. The initial and boundary value problem under consideration is (1a), (1b), (1c), (4), (5), (6), (2a), (2b), (3).

Dependency of the mutation rates on the mean radius. To keep feedback mechanisms description tractable, we assume that the differentiation rates β and β' are functions of the mean radius $\bar{r}(t)$ at time t . As said above, $\int_{r_*}^{r_c} a(t, s) ds$ represents the total number of adipocytes, at time t . The mean radius of adipocytes at time t is therefore equal to:

$$\bar{r}(t) = \frac{\int_{r_*}^{r_c} s a(t, s) ds}{\int_{r_*}^{r_c} a(t, s) ds} \quad (4)$$

and we also introduce for further purposes

$$S(t) = 4\pi \int_{r_*}^{r_c} s^2 a(t, s) ds, \quad (5)$$

the total surface of the adipocytes at time t .

We define β and β' as functions of \bar{r} , typically with a sigmoid shape that reproduces threshold effects:

$$\beta(\bar{r}) = \beta_m + \frac{\beta_M - \beta_m}{1 + e^{-\frac{\bar{r} - r_\beta}{R_\beta}}} \quad \text{and} \quad \beta'(\bar{r}) = \beta'_m + \frac{\beta'_M - \beta'_m}{1 + e^{-\frac{\bar{r} - r_{\beta'}}{R_{\beta'}}}}$$

with all parameters positive and such that $\beta_M \geq \beta_m$, $\beta'_M \geq \beta'_m$. The image of β is $[\beta_m, \beta_M]$; the sigmoid β is "centered" on r_β and its slope at mid height is $\frac{\beta_M - \beta_m}{4R_\beta}$. The behavior of β' relatively to its parameters is similar, see Figure 1 for a typical shape. In particular, from a mathematical point of view, β and β' are bounded

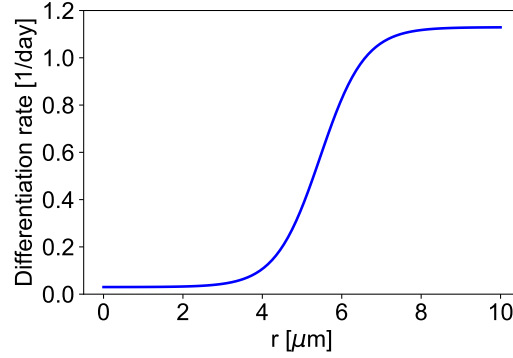


FIGURE 1. Shape of β and β' as functions of the radius.

Lipschitz-continuous functions.

Description of the growth rate. The dynamics of the radius of an adipocyte $t \rightarrow R(t)$ with respect to time can be approximated with the ODE

$$\frac{d}{dt}R(t) = V(t, R(t)),$$

where V is the growth rate. We assume that adipocytes capture all the excess of food, i.e. not used by the metabolism. Adipocytes gather the food through their membranes, thus the flux of food they receive is proportional to their surface. Given a radius $r_* < R < r_c$ the flux of food is proportional to the ratio of the surface of the considered adipocyte over the total surface of all the adipocytes, that is

$$k \frac{R^2}{\int_{r_*}^{r_c} s^2 a(t, s) ds}$$

where $k > 0$ is the (excess of) available food. In the present paper, k is constant in time, but it could be relevant to consider it as evolving in time, for example with time periodic food input to mimic circadian cycle. Thus, in the time interval $[t, t + dt]$, the volume variation of such an adipocyte with radius $R(t)$ is governed by

$$\mathcal{V}(t + dt) = \mathcal{V}(t) + k \frac{R(t)^2}{\int_{r_*}^{r_c} s^2 a(t, s) ds} \times dt.$$

Letting dt go to 0, we deduce that the volume obeys the ODE $\frac{d\mathcal{V}}{dt} = k \frac{R(t)^2}{\int_{r_\star}^{r_c} s^2 a(t, s) ds}$. Since the volume $\mathcal{V}(t)$

is related to the radius $R(t)$ by $\mathcal{V}(t) = \frac{4}{3}\pi R(t)^3$, we end up with

$$\frac{d\mathcal{V}}{dt} = 4\pi R(t)^2 \frac{dR}{dt} = 4\pi R(t)^2 \times V(t, R(t)) = k \frac{R(t)^2}{\int_{r_\star}^{r_c} s^2 a(t, s) ds}.$$

Consequently, we have

$$V(t, r) = \frac{k}{4\pi \int_{r_\star}^{r_c} s^2 a(t, s) ds} = \frac{k}{S(t)}.$$

This relation holds as far as the radius is not too large. As already mentioned above, the size of the adipocytes is limited. There are several possibilities to model such a threshold, based either on phenomenological arguments, or on energetic considerations. In what follows, we make the equation as simple as possible, with the formula

$$V(t, r) = \frac{k}{S(t)} \mathbb{1}_{[r_\star, r_c)}(r) \quad (6)$$

which assumes that the growth rate vanishes outside the domain $r \in [r_\star, r_c]$. This simple definition will allow us to derive easily interesting formula for the stationary solutions of the model.

However, for the numerical simulations, we adopt the following regularized growth rate :

$$V(t, r) = \frac{k}{S(t)} \mathbb{1}_{[r_\star, r_c - \epsilon)}(r) - \frac{r - r_c}{\epsilon} \frac{k}{S(t)} \mathbb{1}_{[r_c - \epsilon, r_c)}(r),$$

where $\epsilon > 0$ is a small parameter.

Typical values for the parameters are collected in Table 2.

1.2. Definition of the solutions to system (1)-(3)

The definition (6) of the growth rate V raises some slight technical difficulties. Indeed, the equation for the adipocytes concentration $(t, r) \mapsto a(t, r)$ is a transport equation, which is classically understood by means of the characteristic curves associated with the growth rate $V(t, r)$. However, V , as given by (6), does not fulfill the regularity required to apply the Cauchy-Lipschitz theorem. Nevertheless, assuming that $S(t) \geq \epsilon > 0$ for all $t \in [0, T)$, V satisfies the following one sided Lipschitz condition (OSLC):

for all $r_1, r_2 \in [r_\star, +\infty)$, for all $0 \leq t \leq T < \infty$, $(V(t, r_1) - V(t, r_2))(r_1 - r_2) \leq C(t)|r_1 - r_2|^2$ with $C \in L^1(0, T)$.

Hence, we can appeal to the generalized theory introduced by A. Filippov [10], see also [14] for an application to transport equations with discontinuous coefficients. It allows us to consider the family of continuous Filippov maps

$$X_t : ([0, t] \times \{r_\star\}) \cup (\{0\} \times [r_\star, +\infty)) \rightarrow [r_\star, +\infty),$$

satisfying $X_s(s, r_\star) = r_\star$ for all $s \in [0, t]$, $X_0(0, r) = r$ for all $r \in [r_\star, +\infty)$ and, for fixed $(s, r) \in (0, \infty) \times (r_\star, \infty)$, the function $t \mapsto X_t(s, r)$ is absolutely continuous on $[s, \infty)$ and satisfies the differential equation $\frac{d}{dt} X_t = V(t, X_t)$ for almost every t with Cauchy datum $X_s(s, r) = r$. Owing to the OSLC, X_t is the unique flow of the differential equation for $t \geq s$.

In our particular case, the characteristic maps associated with a given S can be explicitly computed and are defined by:

$$X_t^S(0, r) = \min \left(r + \int_0^t \frac{k}{S(u)} du, r_c \right), \quad t \geq 0, \quad X_t^S(s, r_*) = \min \left(r_* + \int_s^t \frac{k}{S(u)} du, r_c \right), \quad t \geq s \geq 0. \quad (7)$$

Note that any trajectory issued from $r \in [r_*, r_c]$ do not cross the line $r = r_c$: sizes larger than r_c cannot be reached, which corresponds to the intuition since the velocity vanishes of (r_c, ∞) . Moreover, there is no need of boundary condition for the transport equation for the adipocytes at $r = r_c$ since there is nothing entering from this end into the domain.

Let a_0 be a positive finite measure supported on $[r_*, r_c]$. We denote by $\mathcal{M} - w*$ the set of finite measures on $[r_*, +\infty)$ endowed with the weak star topology.

We generalize Eq.(3) by replacing its right-hand side with a given positive continuous function $f \in C^0(\mathbb{R}_+)$. In that context, we will call a solution to the problem (1c)-(2b)-(3) with initial condition, i.e.

$$\begin{cases} \partial_t a(t, r) + \partial_r (Va)(t, r) = -\gamma'' a(t, r), & t > 0, r > r_*, \\ V(t, r_*) a(t, r_*) = f(t), & t > 0, \\ a(0, r) = a_0(r), & r > r_* \end{cases} \quad (8)$$

any measure-valued function $a \in C^0(\mathbb{R}_+; \mathcal{M} - w*)$ such that the following Duhamel formula holds: for all $\phi \in C_b^0([r_*, +\infty))$ and for all $t \in [0, T]$,

$$\int_{r_*}^{+\infty} \phi(r) da_t(r) = \int_0^t e^{-\gamma''(t-s)} \phi(X_t^S(s, r_*)) f(s) ds + \int_{r_*}^{+\infty} e^{-\gamma''t} \phi(X_t^S(0, r)) da_0(r) \quad (9)$$

where $T = \inf\{t : S(t) = 0\}$.

Note that here, a_t denotes the measure a at time t and the condition $a \in C^0(\mathbb{R}_+; \mathcal{M} - w*)$ means that

$$\lim_{h \rightarrow 0} \int \phi(r) da_{t+h}(r) = \int \phi(r) da_t(r)$$

holds for any continuous and bounded trial function ϕ . In the following, we shall use the definition (9) with $f(t) = \beta'(\bar{r}(t))p(t)$. Moreover, we bear in mind that the problem is non linear, since the growth rate V depends on the total surface $S(t)$ of the adipocytes, see (5). It turns out that the OSLC on which the construction is based relies on the positivity of S , that we are going to discuss now, showing that the lifespan of solution is infinite (for positive times).

Bearing in mind the physical meaning of the unknown, the data f and a_0 are non negative, with, furthermore, $\text{supp}(a_0) \subset [r_*, r_c]$. Formula (9) then tells us that a_t is a non negative measure too. We also remark that the characteristics issued from $[r_*, r_c]$ cannot exceed r_c (this is a consequence of the well-posedness of this Filippov-type Cauchy problem) and

$$\forall t \in [0, T), \quad X_t^S(\left([0, t] \times \{r_*\}\right) \cup (\{0\} \times [r_*, +\infty))) \subset [r_*, r_c].$$

Accordingly, the support of a_t remains in $[r_*, r_c]$ for all $t \in [0, T)$. Finally, let us discuss formally that the model does not produce a shrinking of the surface, that would be an obstacle to the global existence of solutions. Since a_t is compactly supported, we can use (9) with $\phi(r) = 4\pi r^2$ to compute the surface as:

$$S(t) = 4\pi \left(e^{-\gamma''t} \int_{r_*}^{r_c} (X_t^S(0, r))^2 da_0(r) + \int_0^t e^{-\gamma''(t-s)} (X_t^S(s, r_*))^2 f(s) ds \right). \quad (10)$$

This formula enables to bound from below the value of $S(t)$ as

$$\forall t \in [0, T], \quad S(t) = 4\pi \int_{r_\star}^{+\infty} r^2 da_t(r) = 4\pi \int_{r_\star}^{r_c} r^2 da_t(r) \geq 4\pi r_\star^2 e^{-\gamma''t} a_0([r_\star, r_c]).$$

The continuity of S , which comes from the continuity of $t \mapsto a_t$, enables to conclude that $T = +\infty$.

1.3. Outline of the article

In this article, a complete study of the model is proposed: in section 2, we begin with a computation of the stationary solutions of the model, followed by a proof of the existence and uniqueness of solutions in Section 3. The asymptotic in time behavior of the system is described in Section 4 and some numerical simulations are displayed in Section 5. Finally, this model is extended by considering space heterogeneities through a coupling with a fluid environment and numerical simulations are presented in Section 6.

2. STATIONARY SOLUTIONS

We will use the previous framework to exhibit stationary solutions of the system (1)-(3). Finding a stationary solution (m, p, a_0) is equivalent to finding a solution for the following system:

$$\begin{cases} (\delta - \beta(\bar{r}))m = 0 \\ (\delta' - \beta'(\bar{r}))p + \beta(\bar{r})m = 0 \\ Va(r_\star) = \beta'(\bar{r})p, \quad \text{with } V = \frac{k}{S}, \\ \int_{r_\star}^{+\infty} \phi(r) da_0(r) = \int_0^t e^{-\gamma''(t-s)} \phi(X_t^S(s, r_\star)) \beta'(\bar{r})p ds + \int_{r_\star}^{+\infty} e^{-\gamma''t} \phi(X_t^S(0, r)) da_0(r) \end{cases} \quad (11)$$

for all $\phi \in \mathcal{C}_b^0([r_\star, +\infty))$ and for all $t \in [0, +\infty)$, with unknowns a_0 a positive finite measure supported on $[r_\star, r_c]$ and $m, p \in [0, +\infty)$. The last condition expresses the fact that $a_t = a_0$ for all $t \in [0, +\infty)$ where a is a solution in the sense given in the previous section.

Let (m, p, a_0) be a solution to (11) and $V = \frac{k}{S}$. The characteristics X_t^S are computed using the constant function $S = 4\pi \int_{r_\star}^{r_c} r^2 da_0(r)$ and are well defined since a_0 is positive, that is to say:

$$X_t^S(s, r_\star) = \min(r_\star + V(t-s), r_c) \quad \text{and} \quad X_t^S(0, r) = \min(r + Vt, r_c).$$

We can hence rewrite the last equation of system (11) at time $t = \frac{r_c - r_\star}{V}$ as

$$\int_{r_\star}^{r_c} \phi(r) da_0(r) = \frac{\beta'(\bar{r})p}{V} \int_{r_\star}^{r_c} e^{-\frac{\gamma''}{V}(u-r_\star)} \phi(u) du + e^{-\frac{\gamma''}{V}(r_c-r_\star)} \phi(r_c) a_0([r_\star, r_c]). \quad (12)$$

Using the equality $a(r_\star) = \frac{\beta'(\bar{r})p}{V}$, we deduce the form of a_0 as:

$$a_0 = a(r_\star) e^{-\frac{\gamma''}{V}(r-r_\star)} \mathbb{1}_{[r_\star, r_c]} dr + \mu \delta_{r_c},$$

where μ can be determined from (12) through the relation:

$$\mu = \int_{r_\star}^{r_c} a(r_\star) e^{-\frac{\gamma''}{V}(r-r_\star)} e^{-\frac{\gamma''}{V}(r_c-r_\star)} dr + \mu e^{-\frac{\gamma''}{V}(r_c-r_\star)}$$

and finally we find

$$\mu = \frac{V}{\gamma''} a(r_*) e^{-\frac{\gamma''}{V}(r_c - r_*)}.$$

Therefore the stationary solutions satisfy

$$\begin{cases} (\delta - \beta(\bar{r})) m = 0 \\ (\delta' - \beta'(\bar{r})) p + \beta(\bar{r}) m = 0 \\ Va(r_*) = \beta'(\bar{r}) p, \quad \text{with } V = \frac{k}{S}, \\ a_0 = a(r_*) e^{-\frac{\gamma''}{V}(r - r_*)} \mathbb{1}_{[r_*, r_c]} dr + \frac{V}{\gamma''} a(r_*) e^{-\frac{\gamma''}{V}(r_c - r_*)} \delta_{r_c}, \end{cases} \quad (13)$$

with unknowns $p, m \in \mathbb{R}_+$, $a(r_*) \in \mathbb{R}_+^*$.

Note that the expression for a_0 enables to compute \bar{r} and S as functions of V , i.e.:

$$\bar{r} = \frac{\int_{r_*}^{r_c} s da_0(s)}{\int_{r_*}^{r_c} da_0(s)} = \frac{\gamma''}{V} \int_{r_*}^{r_c} r e^{-\frac{\gamma''}{V}(r - r_*)} dr + r_c e^{-\frac{\gamma''}{V}(r_c - r_*)} = r_* + \frac{V}{\gamma''} (1 - e^{-\frac{\gamma''}{V}(r_c - r_*)})$$

and

$$\begin{aligned} S &= 4\pi \int_{r_*}^{r_c} s^2 da_0(s) = 4\pi a(r_*) \left(\int_{r_*}^{r_c} r^2 e^{-\frac{\gamma''}{V}(r - r_*)} dr + r_c^2 \frac{V}{\gamma''} e^{-\frac{\gamma''}{V}(r_c - r_*)} \right) \\ &= 4\pi a(r_*) \left(\frac{V}{\gamma''} r_*^2 - 2 \left(\frac{V}{\gamma''} \right)^2 \left(r_c e^{-\frac{\gamma''}{V}(r_c - r_*)} - r_* \right) + 2 \left(\frac{V}{\gamma''} \right)^3 \left(1 - e^{-\frac{\gamma''}{V}(r_c - r_*)} \right) \right). \end{aligned} \quad (14)$$

Proposition 1. *System (13) has a non-trivial (i.e. with a non-zero a_0) solution if and only if one of the following two conditions hold:*

- (1) $\delta' \in \beta'((r_*, r_c))$,
- (2) $\delta \in \beta((r_*, r_c))$ and $\delta' - \beta'(\beta^{-1}(\delta)) < 0$.

Proof. We begin with noticing that p cannot be zero, since it would imply that $a(r_*) = 0$ and therefore $a_0 = 0$.

Now, remark that the function Ψ such that $\bar{r} = \Psi(V)$ and defined by $\Psi : V \rightarrow r_* + \frac{V}{\gamma''} (1 - e^{-\frac{\gamma''}{V}(r_c - r_*)})$ is strictly increasing on \mathbb{R}_+^* and satisfies $\lim_{V \rightarrow 0^+} \Psi(V) = r_*$ and $\lim_{V \rightarrow +\infty} \Psi(V) = r_c$.

Assume that there exists a non-trivial solution. If $m = 0$, we should impose that $\delta' \in \beta'((r_*, r_c))$. If $m \neq 0$, then $m > 0$ (we are interested in physical solutions) and it implies that $\delta \in \beta((r_*, r_c))$, namely $\delta = \beta(\bar{r})$ with \bar{r} such that $\delta' - \beta'(\bar{r}) = -\beta(\bar{r})m/p < 0$. thus if there exists a non-trivial solution, one of the two conditions is satisfied.

Conversely, if $\delta' \in \beta'((r_*, r_c))$, we find a stationary solution defined by

$$\bar{r} = \beta'^{-1}(\delta'), \quad m = 0, \quad V = \Psi^{-1}(\bar{r}), \quad S = \frac{k}{V}.$$

From Eq.(14), we can deduce the value of $a(r_*)$ knowing S and V , and therefore a_0 and $p = \frac{Va(r_*)}{\beta'(\bar{r})}$.

Similarly, if $\delta \in \beta((r_*, r_c))$ and $\delta' - \beta'(\beta^{-1}(\delta)) < 0$, then a solution is given by

$$\bar{r} = \beta^{-1}(\delta), \quad V = \Psi^{-1}(\bar{r}), \quad S = \frac{k}{V}, \quad a(r_*) \text{ from Eq.(14)}, \quad p = \frac{Va(r_*)}{\beta'(\bar{r})}, \quad m = \frac{-(\delta' - \beta'(\bar{r}))}{\beta(\bar{r})}p.$$

□

Remark 1. *The stationary solution may not be unique. Precisely, if exactly one condition is fulfilled, the stationary solution is unique. However, if both conditions are fulfilled, we may have two different values of \bar{r} and thus two different stationary solutions: one with $m = 0$ and another one with $m > 0$. If one sees stationary solutions as asymptotic in time unsteady solutions, the non-uniqueness of stationary solutions is understood as the existence of different limit profiles with different initial conditions. We do not address here the problem of the stability of the stationary solutions.*

3. EXISTENCE AND UNIQUENESS OF UNSTEADY SOLUTIONS

Equations of system (1)-(3) are coupled altogether as follows: the ODE part of system (1), that is to say equations (1a) - (1b) is a simple linear ODE system, but which coefficients are defined through the mean radius function \bar{r} of adipocytes, defined at Eq.(4). We therefore need to know function a to compute \bar{r} . Conversely, the transport part of system (1), that is to say equation (1c), depends on the total surface S of a through the velocity V defined at Eq. (6) and depends on function p solution to the ODE part, through the boundary condition (3).

In this section, we will prove the existence and uniqueness of solutions to system (1)-(3). To do so, we will proceed in three steps: first we prove, in Subsection 3.1, the existence and uniqueness of solutions to the ODE part (1a) - (1b)-(2a). Then, in Subsection 3.2, we prove the existence and uniqueness of solutions to the transport equation (1c)-(3)-(2b) for a given non negative flux by solving a fixed point equation. We also prove some stability property with respect to the flux that will be used later. Finally, in Subsection 3.3, we prove the existence and uniqueness of a solution to the general system thanks to a fixed-point theorem, coupling the results obtained at the foregoing subsections.

3.1. Some preliminary results on the solution of the ODE part (1a) - (1b)-(2a)

First we will give some existence and stability results on the solution of the ODE part (1a) - (1b) of system (1) with initial conditions (2a), assuming that the mean radius $\bar{r} \in \mathcal{C}^0([0, T], [r_*, r_c])$ is given.

Since β and β' are bounded, the following function:

$$\begin{pmatrix} m \\ p \end{pmatrix} \mapsto \begin{pmatrix} \delta - \beta(\bar{r}(t)) & 0 \\ \beta(\bar{r}(t)) & \delta' - \beta'(\bar{r}(t)) \end{pmatrix} \begin{pmatrix} m \\ p \end{pmatrix}$$

is Lipschitz-continuous. We call L its Lipschitz modulus.

Therefore, the system satisfies the hypotheses of Cauchy-Lipschitz Theorem and we have the following bound:

$$\max(m(t), p(t)) \leq \max(m_0, p_0) \exp(Lt), \quad \text{for all } t \in [0, T]. \quad (15)$$

Moreover, we can prove the following stability property of the solution with respect to \bar{r} , where $p(\bar{r})$ denotes the solution p computed with the mean radius function \bar{r} : for all $\bar{r}_1, \bar{r}_2 \in \mathcal{C}^0([0, T], [r_*, r_c])$,

$$|p(\bar{r}_1)(t) - p(\bar{r}_2)(t)| \leq C \max(m_0, p_0) \|\bar{r}_1 - \bar{r}_2\|_{L^1([0, t])} e^{2Lt}, \quad \text{for all } t \in [0, T]. \quad (16)$$

Indeed, let us denote by M the following Lipschitz-continuous function of Lipschitz modulus k :

$$M(r) = \begin{pmatrix} \delta' - \beta'(r) & \beta(r) \\ 0 & \delta - \beta(r) \end{pmatrix}.$$

We obtain the following inequality, using (15):

$$\begin{aligned} & \left\| \begin{pmatrix} m(\bar{r}_1)(t) - m(\bar{r}_2)(t) \\ p(\bar{r}_1)(t) - p(\bar{r}_2)(t) \end{pmatrix} \right\|_{\infty, \mathbb{R}^2} \\ & \leq \int_0^t \left(k |\bar{r}_1(s) - \bar{r}_2(s)| \left\| \begin{pmatrix} m(\bar{r}_1)(s) \\ p(\bar{r}_1)(s) \end{pmatrix} \right\|_{\infty, \mathbb{R}^2} + \left\| M(\bar{r}_2(s)) \begin{pmatrix} m(\bar{r}_1)(s) - m(\bar{r}_2)(s) \\ p(\bar{r}_1)(s) - p(\bar{r}_2)(s) \end{pmatrix} \right\|_{\infty, \mathbb{R}^2} \right) ds \\ & \leq k \left\| \begin{pmatrix} m_0 \\ p_0 \end{pmatrix} \right\|_{\infty, \mathbb{R}^2} \|\bar{r}_1 - \bar{r}_2\|_{L^1([0,t])} e^{Lt} + \int_0^t L \left\| \begin{pmatrix} m(\bar{r}_1)(s) - m(\bar{r}_2)(s) \\ p(\bar{r}_1)(s) - p(\bar{r}_2)(s) \end{pmatrix} \right\|_{\infty, \mathbb{R}^2} ds \end{aligned}$$

and we conclude thanks to Grönwall's Lemma.

3.2. Solution to the transport equation (1c)-(3)-(2b) with a given non negative flux

In this section, the first theorem gives an existence and uniqueness result for the transport part (1c) of system (1), complemented with boundary condition (3) and initial condition (2b).

Remark that the velocity V , involved in the transport equation (8) and defined at Eq.(6), depends on the total surface S , which is computed thanks to the solution a of Eq. (8). We are therefore led to consider the following fixed-point problem, coming from the expression of the surface S as a function of the characteristic curves X_t^S , see Eq.(10):

$$S(t) = 4\pi \left(e^{-\gamma''t} \int_{r_\star}^{r_c} (X_t^S(0, r))^2 da_0(r) + \int_0^t e^{-\gamma''(t-s)} (X_t^S(s, r_\star))^2 f(s) ds \right) \quad (17)$$

where

$$\begin{aligned} X_t^S(0, r) &= \min \left(r + \int_0^t \frac{k}{S(u)} du, r_c \right), & t \geq 0, \\ X_t^S(s, r_\star) &= \min \left(r_\star + \int_0^t \frac{k}{S(u)} du - \int_0^s \frac{k}{S(u)} du, r_c \right), & t \geq s \geq 0. \end{aligned}$$

It is easy to prove that solutions to Eq. (17) and solutions to Eq. (8) are the same, defining a by the following formula:

$$\int_{r_\star}^{r_c} \phi(r) da_t(r) = e^{-\gamma''t} \int_{r_\star}^{r_c} \phi(X_t^S(0, r)) da_0(r) + \int_0^t e^{-\gamma''(t-s)} \phi(X_t^S(s, r_\star)) f(s) ds,$$

for all $t \in [0, T]$ and for all $\phi \in \mathcal{C}_b^0([r_\star, r_c])$.

Now, let us prove the existence and uniqueness of solutions to system (8).

Theorem 1. *Let $T > 0$, $\gamma'' > 0$, $f \in \mathcal{C}^0([0, T]; \mathbb{R}_+)$ and $a_0 \in \mathcal{M}$ a positive measure supported in $[r_\star, r_c]$. Then, system (8), with V defined at Eq. (6), has a unique solution.*

Proof. As explained before, it is enough to prove the existence and uniqueness of solutions to the fixed-point equation (17).

To do so, we define the following operator Γ on $\mathcal{C}^0([0, T], \mathbb{R}_+^*)$ by:

$$\Gamma(S)(t) = 4\pi \left(e^{-\gamma''t} \int_{r_\star}^{r_c} (X_t^S(0, r))^2 da_0(r) + \int_0^t e^{-\gamma''(t-s)} (X_t^S(s, r_\star))^2 f(s) ds \right), \quad t \in [0, T]. \quad (18)$$

and we prove that Γ is a contraction.

We can prove easily that the range of Γ is $E = \mathcal{C}^0([0, T], [\epsilon(T), +\infty))$, where $\epsilon(T) = 4\pi e^{-\gamma''T} r_\star^2 \int_{r_\star}^{r_c} da_0 > 0$ and, for any $\mu > 0$, we define the following norm on E :

$$\|f\|_E = \sup_{t \in [0, T]} |f(t)| e^{-\mu t}. \quad (19)$$

Then, the following inequality holds, for all $S_1, S_2 \in E$ and for all $t \in [0, T]$:

$$|\Gamma(S_1)(t) - \Gamma(S_2)(t)| \leq 8\pi r_c k \left(\int_{r_*}^{r_c} da_0(r) + \|f\|_{L^1[0,t]} \right) \int_0^t \left| \frac{1}{S_1(s)} - \frac{1}{S_2(s)} \right| ds,$$

which comes from the fact that

$$\left| \left(\min(r + \int_0^t \frac{k}{S_1(s)} ds, r_c) \right)^2 - \left(\min(r + \int_0^t \frac{k}{S_2(s)} ds, r_c) \right)^2 \right| \leq 2r_c k \int_0^t \left| \frac{1}{S_1(s)} - \frac{1}{S_2(s)} \right| ds.$$

Indeed, for any $\lambda, \mu, \nu \in \mathbb{R}$, one has

$$|\min(\lambda, \nu)^2 - \min(\mu, \nu)^2| = |\min(\lambda, \nu) + \min(\mu, \nu)| |\min(\lambda, \nu) - \min(\mu, \nu)| \leq 2|\nu| |\lambda - \mu|.$$

Since

$$\int_0^t \left| \frac{1}{S_1(s)} - \frac{1}{S_2(s)} \right| ds \leq \frac{1}{\mu \epsilon(t)^2} e^{\mu t} \|S_1 - S_2\|_E,$$

we obtain that

$$|\Gamma(S_1)(t) - \Gamma(S_2)(t)| e^{-\mu t} \leq 8\pi r_c k \left(\int_{r_*}^{r_c} da_0(r) + \|f\|_{L^1[0,t]} \right) \frac{1}{\mu \epsilon(t)^2} \|S_1 - S_2\|_E. \quad (20)$$

Thus, if we take μ large enough, the operator Γ is a contraction of the complete metric space $(E, \|\cdot\|_E)$ and the Banach fixed point Theorem proves the existence and uniqueness of the solution to equation (17). \square

We will denote by $S(f)$ the unique solution to equation (17), defined at Theorem 1, with the positive flux condition f . We prove now a stability result, that is to say an estimate of the quantity $|S(f_1)(t) - S(f_2)(t)|$ for $t \in [0, T]$.

Theorem 2. *Let $M \in \mathbb{R}^+$. We have the following estimate: there exists a continuous function $A_M \in C^0([0, T])$ such that for all $t \in [0, T]$, for all $f_1, f_2 \in C^0([0, T], [0, +\infty))$ such that $\|f_1\|_{L^1([0, T])} \leq M$,*

$$|S(f_1)(t) - S(f_2)(t)| \leq A_M(t) \|f_1 - f_2\|_{L^1([0, t])}.$$

Proof. We denote by Γ_1 (respectively Γ_2) the operator defined at Eq.(18) with the flux f_1 (respectively f_2). We decompose the difference $S(f_1) - S(f_2)$ as follows:

$$\begin{aligned} \|S(f_1) - S(f_2)\|_E &= \|\Gamma_1(S(f_1)) - \Gamma_2(S(f_2))\|_E \\ &\leq \|\Gamma_1(S(f_1)) - \Gamma_1(S(f_2))\|_E + \|\Gamma_1(S(f_2)) - \Gamma_2(S(f_2))\|_E. \end{aligned}$$

Using inequality (20), we can bound from above the first term of the right-hand side as follows:

$$\|\Gamma_1(S(f_1)) - \Gamma_1(S(f_2))\|_E \leq \frac{8\pi r_c k}{\mu \epsilon(T)^2} \left(\int_{r_*}^{r_c} da_0(r) + \|f_1\|_{L^1[0, T]} \right) \|S(f_1) - S(f_2)\|_E$$

and taking $\mu = \frac{16\pi r_c k}{\epsilon(T)^2} \left(\int_{r_*}^{r_c} da_0(r) + \|f_1\|_{L^1[0, T]} \right)$, we obtain $\|\Gamma_1(S(f_1)) - \Gamma_1(S(f_2))\|_E \leq \frac{1}{2} \|S(f_1) - S(f_2)\|_E$.

We now control the second term of the right-hand side $\|\Gamma_1(S(f_2)) - \Gamma_2(S(f_2))\|_E$, i.e.:

$$\|\Gamma_1(S(f_2)) - \Gamma_2(S(f_2))\|_E \leq \|\Gamma_1(S(f_2)) - \Gamma_2(S(f_2))\|_{L^\infty([0, T])} \leq 4\pi r_c^2 \|f_1 - f_2\|_{L^1([0, T])}$$

and therefore, using the value of μ and the definition (19) of the norm,

$$|S(f_2)(T) - S(f_1)(T)| \leq 8\pi r_c^2 \exp\left(T \frac{16\pi r_c k}{\epsilon(T)^2} \left(\int_{r_*}^{r_c} da_0(r) + M\right)\right) \|f_1 - f_2\|_{L^1([0, T])}.$$

For any $t \in [0, T]$, applying the previous inequality to the restriction of the solutions to $[0, t]$, we obtain

$$|S(f_2)(t) - S(f_1)(t)| \leq 8\pi r_c^2 \exp\left(t \frac{16\pi r_c k}{\epsilon(t)^2} \left(\int_{r_*}^{r_c} da_0(r) + M\right)\right) \|f_1 - f_2\|_{L^1([0, t])}.$$

□

3.3. Existence and uniqueness of solutions to system (1)-(3).

Now let us prove the following theorem, that states the existence and uniqueness for the full system (1)-(3), coupling the results of the previous two subsections.

Once again, this is equivalent to a fixed-point problem. Indeed, the resolution of the ODE part (1a) - (1b) requires the knowledge of the mean radius \bar{r} , which is computed from the solution a of the transport equation (1c). In turns, the boundary condition (3), which is necessary to compute a , involves the function p , solution of the ODE part.

More precisely, we consider a solution (m, p, a) to system (1)-(3). Knowing a , we can compute the function S thanks to formula (5) and therefore the characteristics X_t^S associated to system (1c)-(2b)-(3) thanks to formula (7).

We can consequently write $\bar{r}(t)$ in the form of a fixed point equation, using formula (4) and Eq.(9) with $f(t) = \beta(\bar{r}(t))p(t)$, that is to say

$$\bar{r}(t) = \frac{e^{-\gamma''t} \int_{r_*}^{r_c} X_t^S(0, r) da_0(r) + \int_0^t e^{-\gamma''(t-s)} X_t^S(s, r_*) \beta(\bar{r}(s)) p(s) ds}{e^{-\gamma''t} \int_{r_*}^{r_c} da_0(r) + \int_0^t e^{-\gamma''(t-s)} \beta(\bar{r}(s)) p(s) ds}. \quad (21)$$

Conversely, if we find a function \bar{r} , solution to Eq.(21), we can then solve the ODE part (1a) - (1b)-(2a) of system (1) in order to obtain functions m and p , see Subsection 3.1. We can then deduce surface S from the fixed point equation (17) with $f(t) = \beta'(\bar{r}(t)) p(t)$, that is to say, following the notation of Sec. 3.2, $S = S(\beta'(\bar{r}) p)$. Solution a is finally given by Eq. (9).

We are therefore reduced to find a solution to the fixed point problem (21) with p solution to Eq. (1b) and $S = S(\beta'(\bar{r}) p)$.

Now, let us prove the existence and uniqueness of solutions to system (1)-(3).

Theorem 3. *Let $m_0 \geq 0$, $p_0 \geq 0$, $a_0 \in \mathcal{M}$ with a_0 a positive measure supported in $[r_*, r_c]$. Then, for any $0 < T < \infty$, the system (1)-(3) has a unique solution $(m, p, a) \in \mathcal{C}^1([0, T], [0, +\infty))^2 \times \mathcal{C}^0([0, T], \mathcal{M} - w^*)$.*

Proof. As explained before, we are reduced to find a solution to the fixed point problem (21) with p solution to Eq. (1b) and $S = S(\beta'(\bar{r}) p)$. To do so, let $0 < T < \infty$ and define the following operator: $\Lambda : \mathcal{C}^0([0, T], [r_*, r_c]) \rightarrow \mathcal{C}^0([0, T], [r_*, r_c])$:

$$\Lambda(\bar{r})(t) = \frac{e^{-\gamma''t} \int_{r_*}^{r_c} X_t^S(0, r) da_0(r) + \int_0^t e^{-\gamma''(t-s)} X_t^S(s, r_*) \beta(\bar{r}(s)) p(s) ds}{e^{-\gamma''t} \int_{r_*}^{r_c} da_0(r) + \int_0^t e^{-\gamma''(t-s)} \beta(\bar{r}(s)) p(s) ds} \quad \text{for all } t \in [0, T], \quad (22)$$

where $S = S(\beta'(\bar{r}) p)$.

To prove the contraction of operator Λ , we will use the same idea and the same norm (19) than previously. We will also need the stability results demonstrated at subsections 3.1 and 3.2.

Let $F = \mathcal{C}^0([0, T], [r_*, r_c])$. We will prove in the following that there exists $A > 0$ (which may depend on T) such that for all $\bar{r}_1, \bar{r}_2 \in F$ and for all $t \in [0, T]$,

$$|\Lambda(\bar{r}_1)(t) - \Lambda(\bar{r}_2)(t)| \leq A \int_0^t |\bar{r}_1(u) - \bar{r}_2(u)| \, du. \quad (23)$$

Therefore,

$$|\Lambda(\bar{r}_1)(t) - \Lambda(\bar{r}_2)(t)| \leq A \int_0^t \|\bar{r}_1 - \bar{r}_2\|_F e^{\mu u} \, du \leq \frac{A}{\mu} \|\bar{r}_1 - \bar{r}_2\|_F e^{\mu t}$$

and finally, if we take μ large enough, Λ is a contraction of the complete metric space $(F, \|\cdot\|_F)$. Thus the Banach fixed-point theorem gives the existence and uniqueness of the solution to the fixed point equation (21).

Now let us prove inequality (23). Considering the definition (22) of operator Λ , it is sufficient to prove that the following three functions are Lipschitz-continuous and bounded with respect to \bar{r} in $L^1([0, t])$:

- (1) $\bar{r} \mapsto e^{-\gamma''t} \int_{r_*}^{r_c} da_0(r) + \int_0^t e^{-\gamma''(t-s)} \beta(\bar{r}(s)) p(s) \, ds$,
- (2) $\bar{r} \mapsto e^{-\gamma''t} \int_{r_*}^{r_c} X_t^S(0, r) \, da_0(r)$ where $S = S(\beta'(\bar{r}) p)$,
- (3) $\bar{r} \mapsto \int_0^t e^{-\gamma''(t-s)} X_t^S(s, r_*) \beta(\bar{r}(s)) p(s) \, ds$ where $S = S(\beta'(\bar{r}) p)$.

First, using the fact that β' is a bounded Lipschitz-continuous function, the bound (15) and the stability property (16) regarding the solution p of the ODE part (1b), it is straightforward to prove that for all $\bar{r}_1, \bar{r}_2 \in F$, for all $t \in [0, T]$,

$$\|\beta'(\bar{r}_1)p(\bar{r}_1) - \beta'(\bar{r}_2)p(\bar{r}_2)\|_{L^1([0, t])} \leq B \|\bar{r}_1 - \bar{r}_2\|_{L^1([0, t])}, \quad (24)$$

where $p(\bar{r})$ denotes the solution p of Eq. (1b) computed with the given mean radius function \bar{r} .

Function (1): Function $\bar{r} \mapsto e^{-\gamma''t} \int_{r_*}^{r_c} da_0(r) + \int_0^t e^{-\gamma''(t-s)} \beta(\bar{r}(s)) p(s) \, ds$ is therefore clearly bounded from below and above and Lipschitz-continuous.

Function (2): Function $\bar{r} \mapsto e^{-\gamma''t} \int_{r_*}^{r_c} X_t^S(0, r) \, da_0(r)$ is bounded from above by $r_c \int_{r_*}^{r_c} da_0(r)$.

Let $\bar{r}_1, \bar{r}_2 \in F$. Using the expression (7) of the characteristic curves, we obtain that

$$\begin{aligned} \left| X_t^{S(\beta'(\bar{r}_1) p_1)}(0, r) - X_t^{S(\beta'(\bar{r}_2) p_2)}(0, r) \right| &\leq \int_0^t \left| \frac{k}{S(\beta'(\bar{r}_1) p(\bar{r}_1))} - \frac{k}{S(\beta'(\bar{r}_2) p(\bar{r}_2))} \right| \, ds \\ &\leq \frac{k}{\epsilon(T)^2} \int_0^t |S(\beta'(\bar{r}_1) p(\bar{r}_1))(s) - S(\beta'(\bar{r}_2) p(\bar{r}_2))(s)| \, ds. \end{aligned}$$

Since $\beta'(\bar{r}_1)p(\bar{r}_1)$ and $\beta'(\bar{r}_2)p(\bar{r}_2)$ are bounded, see the properties of β' and Eq. (15), we can use Theorem 2 and inequality (24) to obtain that

$$\begin{aligned} \left| X_t^{S(\beta'(\bar{r}_1) p_1)}(0, r) - X_t^{S(\beta'(\bar{r}_2) p_2)}(0, r) \right| &\leq \frac{k}{\epsilon(T)^2} \int_0^t A_N(s) \|\beta'(\bar{r}_1)p(\bar{r}_1) - \beta'(\bar{r}_2)p(\bar{r}_2)\|_{L^1([0, s])} \, ds \\ &\leq C \|\bar{r}_1 - \bar{r}_2\|_{L^1([0, t])}, \end{aligned}$$

which implies that function $\bar{r} \mapsto e^{-\gamma''t} \int_{r_*}^{r_c} X_t^S(0, r) \, da_0(r)$ is Lipschitz-continuous.

Function (3): A similar proof enables to prove that function $\bar{r} \mapsto \int_0^t e^{-\gamma''(t-s)} X_t^S(s, r_*) \beta(\bar{r}(s)) p(s) \, ds$ is bounded from above and Lipschitz-continuous. \square

4. ASYMPTOTIC BEHAVIOR OF THE SOLUTIONS IN SOME SIMPLE DEGENERATE CASES

In this section, the behavior of the solutions for large times is studied. We first prove that, under some conditions involving the growth rate and the differentiation rate, the number of mesenchymal cells (resp. of

preadipocytes) goes either to zero or to infinity. We distinguish two situations depending whether or not the death rate γ'' of the adipocytes vanishes. In the case $\gamma'' \neq 0$, we prove that the mean radius converges towards the minimal radius as time goes to infinity. In the case $\gamma'' = 0$, we prove that the number of adipocytes converges towards a Dirac mass at r_c .

In some simple cases, we can therefore study the asymptotic behavior of the solution, solving explicitly Eq. (1a) and (1b) as:

$$\begin{aligned} m(t) &= m_0 \exp\left(\delta t - \int_0^t \beta(\bar{r}(s)) \, ds\right), \\ p(t) &= p_0 \exp\left(\delta' t - \int_0^t \beta'(\bar{r}(s)) \, ds\right) + \int_0^t \exp\left(\delta(t-s) - \int_s^t \beta'(\bar{r}(u)) \, du\right) \beta(\bar{r}(s)) m(s) \, ds. \end{aligned}$$

For the proof of the asymptotic properties, we also introduce the zeroth and the first momentum of a_t , that is to say:

$$M_0(t) = \int_{r_\star}^{r_c} da_t(s), \quad M_1(t) = \int_{r_\star}^{r_c} s \, da_t(s). \quad (25)$$

Note that $\bar{r}(t) = \frac{M_1(t)}{M_0(t)}$. We also have the following formula linking the zeroth and the first momenta of a :

$$M_0(t) = M_0(0)e^{-\gamma'' t} + \int_0^t e^{-\gamma''(t-s)} \beta' \left(\frac{M_1(s)}{M_0(s)} \right) p(s) \, ds. \quad (26)$$

We have therefore the following proposition regarding the asymptotic behavior of m and p :

Proposition 2. *Let $m_0 \geq 0$, $p_0 \geq 0$, $a_0 \in \mathcal{M} - w*$ with a_0 positive. We denote by m, p, a_t the solution given by Theorem 3. We have the following limits when $t \rightarrow +\infty$:*

- (1) if $\delta - \beta(r_c) > 0$, then $m \rightarrow +\infty$,
- (2) if $\delta - \beta(r_\star) < 0$, then $m \rightarrow 0$,
- (3) if $m \rightarrow 0$ and if $\delta' - \beta'(r_\star) < 0$, then $p \rightarrow 0$,
- (4) if $m \rightarrow 0$ and if $\delta' - \beta'(r_c) > 0$, then $p \rightarrow +\infty$.

Moreover, If $\delta - \beta(r_\star) < 0$ and $\delta' - \beta'(r_\star) < 0$, then there exist $C > 0$ and $\epsilon > 0$ such that

$$p(t) \leq C e^{-\epsilon t}, \quad \forall t \in [0, +\infty). \quad (27)$$

Proof. First of all, as $r_\star \leq \bar{r}(s) \leq r_c$ for any $s \in [0, +\infty)$, we have the following inequality on m :

$$m_0 \exp((\delta - \beta(r_c))t) \leq m(t) \leq m_0 \exp((\delta - \beta(r_\star))t) \quad \forall t \in [0, +\infty), \quad (28)$$

which gives a limit for m in the two cases $\delta - \beta(r_c) > 0$ and $\delta - \beta(r_\star) < 0$.

In the same manner, when $m \rightarrow 0$, we can use the explicit expression to bound p as follows:

$$p_0 \exp((\delta' - \beta'(r_c))t) \leq p(t) \leq (p_0 + o(\exp(-\delta' + \beta'(r_\star))t)) \exp((\delta' - \beta'(r_\star))t), \quad \forall t \in [0, +\infty).$$

Now, we denote by $\rho = -(\delta - \beta(r_\star))$ and $\rho' = -(\delta' - \beta'(r_\star))$ and we assume that $\rho > 0, \rho' > 0$. Thanks to (28), we obtain that $m(t) \leq m_0 e^{-\rho t}$, $\forall t \in [0, +\infty)$, and we use this bound in the formula for p , leading to:

$$p(t) \leq p_0 e^{-\rho' t} + \int_0^t e^{-\rho'(t-s)} \beta(r_c) m_0 e^{-\rho s} \, ds$$

	$\delta - \beta(r_*) < 0$	$\delta - \beta(r_c) > 0$
$\delta' - \beta'(r_*) < 0$	(0, 0)	($+\infty$, ?)
$\delta' - \beta'(r_c) > 0$	(0, $+\infty$)	($+\infty$, $+\infty$)

 TABLE 1. Summary of the asymptotic behaviors of functions $t \rightarrow (m(t), p(t))$

and therefore

$$p(t) \leq p_0 e^{-\rho t} + m_0 t e^{-\rho t}, \text{ if } \rho = \rho',$$

$$p(t) \leq p_0 e^{-\rho' t} + m_0 \frac{e^{-\rho t} - e^{-\rho' t}}{\rho' - \rho}, \text{ if } \rho \neq \rho'.$$

□

The previous proposition can be summarized in Table 1, where the couple in each cell represents $\left(\lim_{t \rightarrow +\infty} m, \lim_{t \rightarrow +\infty} p \right)$.

4.1. Case $\gamma'' \neq 0$

In the case when $\gamma'' \neq 0$, we can make precise the result on the mean radius \bar{r} . More precisely, if the growth of p is exponential, which holds in particular if $\delta' - \beta'(r_c) > 0$, the total surface increases and the velocity decreases; meanwhile, the flux of mass in r_* increases and therefore a large proportion of the mass of adipocytes stays around r_* .

Proposition 3. *We assume that $\gamma'' \neq 0$. We consider m, p, a_t the solution given by Theorem 3 and M_0 the zeroth momentum of a defined at Eq.(25). Then, we have the following limits when $t \rightarrow +\infty$:*

- (1) if $p \rightarrow 0$, then $M_0 \rightarrow 0$,
- (2) if $p \rightarrow +\infty$, then $M_0 \rightarrow +\infty$.

Moreover, if we assume that there exist $\epsilon > 0$ and $C > 0$ such that for all $t \in [0, +\infty)$, $p(t) \geq C e^{\epsilon t}$, then $\lim_{t \rightarrow +\infty} \bar{r}(t) = r_*$.

Proof. If $\gamma'' \neq 0$ and $p \rightarrow 0$ (resp. $p \rightarrow +\infty$) when $t \rightarrow +\infty$, we can use Eq.(26) to deduce that $M_0 \rightarrow 0$ (resp. $M_0 \rightarrow +\infty$).

Now, let us assume that $p(t) \geq C e^{\epsilon t}$, for all $t \in [0, +\infty)$. First we will prove that the surface increases exponentially, as follows:

$$S(t) \geq r_*^2 M_0(t) \geq C r_*^2 e^{-\gamma'' t} \int_0^t e^{\gamma'' s} \beta'(r_*) e^{\epsilon s} ds.$$

In particular, for t large enough, there exists $C > 0$ such that

$$S(t) \geq C e^{\epsilon t/2}$$

and therefore, since $r_* < r_c$, we have for t large enough that:

$$\min(r_* + \int_s^t \frac{k}{S(u)} du, r_c) = r_* + \int_s^t \frac{k}{S(u)} du \in [r_*, r_* + K e^{-\epsilon t/2}]. \quad (29)$$

Now, from the expression of the mean radius (21) and of the characteristics (7), we get the following equivalent when $t \rightarrow +\infty$:

$$\bar{r}(t) \sim \frac{\int_0^t e^{\gamma'' s} \min(r_* + \int_s^t \frac{k}{S(u)} du, r_c) \beta'(\bar{r}(s)) p(s) ds}{\int_0^t e^{\gamma'' s} \beta'(\bar{r}(s)) p(s) ds},$$

which leads to $\lim_{t \rightarrow +\infty} \bar{r}(t) = r_*$ using Eq.(29). □

4.2. Case $\gamma'' = 0$

Now, in this section, we consider the case $\gamma'' = 0$. At first sight this assumption on the death rate might appear biologically questionable. However, it is very relevant. Indeed, adipocytes have usually a very low mortality (for humans, the renewal of half of the population is about 8 years), see [19]. This could be different for certain specific experiments performed on mice, due to experimental conditions that can enhance the adipocytes mortality. The results on p and m of the previous section still hold but the results on M_0 are different. We prove that in the case when $\delta - \beta(r_*) < 0$ and $\delta' - \beta'(r_*) < 0$, the number of adipocytes converges towards a Dirac mass at r_c .

Proposition 4. *We assume that $\gamma'' = 0$, $\delta - \beta(r_*) < 0$ and $\delta' - \beta'(r_*) < 0$. We consider m, p, a_t the solution given by Theorem 3 and M_0 the zeroth momentum of a defined at Eq.(25). Then, we have the following limits when $t \rightarrow +\infty$:*

$$\lim_{t \rightarrow +\infty} M_0(t) = M_0(0) + \int_0^{+\infty} \beta'(\bar{r}(s)) p(s) ds < +\infty$$

and

$$a_t \xrightarrow{*} \left(M_0(0) + \int_0^{+\infty} \beta'(\bar{r}(s)) p(s) ds \right) \delta_{r_c}.$$

Proof. The integrability of $\beta'(\bar{r}(s)) p(s)$ comes from the exponential decay of p , see Eq. (27), and the limit for $M_0(t)$ when $t \rightarrow +\infty$ comes directly from the expression of M_0 at Eq.(26) with $\gamma'' = 0$.

Let us denote this limit by $M_{0,\infty} = M_0(0) + \int_0^{+\infty} \beta'(\bar{r}(s)) p(s) ds$. Since the total surface $S(t) \leq r_c^2 M_{0,\infty}$, we can deduce that S is bounded from above and therefore that $\int_0^{+\infty} \frac{k}{S(u)} du = +\infty$. Therefore, for t large enough, we can define $s_c(t)$ as the unique real such that

$$\int_{s_c(t)}^t \frac{k}{S(u)} du = r_c - r_*.$$

Since S is bounded from above, we can deduce that $\lim_{t \rightarrow +\infty} s_c(t) = +\infty$.

Let $\phi \in \mathcal{C}^0([r_*, r_c])$. For t large enough, Eq. (9) can be written as:

$$\int_{r_*}^{r_c} \phi(r) da_t(r) = \phi(r_c) \int_{r_*}^{r_c} da_0(r) + \phi(r_c) \int_0^{s_c(t)} \beta'(\bar{r}(s)) p(s) ds + \int_{s_c(t)}^t \phi\left(r_* + \int_s^t \frac{k}{S(u)} du\right) \beta'(\bar{r}(s)) p(s) ds.$$

Moreover using

$$\left| \int_{s_c(t)}^t \phi\left(r_* + \int_s^t \frac{k}{S(u)} du\right) \beta'(\bar{r}(s)) p(s) ds \right| \leq \|\phi\|_\infty \int_{s_c(t)}^{+\infty} \beta'(\bar{r}(s)) p(s) ds,$$

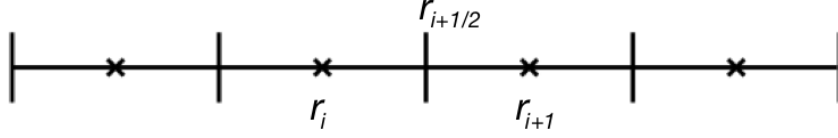


FIGURE 2. Discretization of the interval. The variable a is computed in the middle of each interval, as well as the velocity.

we can compute the limit and we get:

$$\lim_{t \rightarrow +\infty} \int_{r_*}^{r_c} \phi(r) da_t(r) = M_{0,\infty} \phi(r_c),$$

which ends the demonstration. \square

5. NUMERICAL SIMULATIONS

5.1. Numerical scheme

To find a numerical solution to the system of equations, we apply an explicit Euler scheme for the time approximation and an upwind scheme for the discretization of the transport-like equation of the adipocytes population.

We consider a grid with a uniform radius-step $\Delta r > 0$ (see Figure 2) and J intervals. The time step is denoted by Δt . The time step is not constant and it is updated at each iteration according to the Courant-Friedrichs-Lewy stability condition, that will be described later on. Nevertheless, for the sake of simplicity, we denote it by Δt instead of Δt^n .

Let us denote by m^n, p^n the approximations of the solutions $m(t^n)$ and $p(t^n)$ at time t^n . Moreover, a_j^n stands for the approximation of $a(t^n, r_j)$ at time t^n and point r_j and $V_{j+1/2, j \in \{0, \dots, J\}}^n$ is the approximation of the velocity at time t^n at the cells boundaries.

Given the solutions $(m^n, p^n, a_{j \in \{1, \dots, J\}}^n)$ and the velocity $V_{j+1/2, j \in \{0, \dots, J\}}^n$ at time t^n , the solution at time t^{n+1} is updated by

$$\begin{aligned} m^{n+1} &= m^n + \Delta t(\alpha(\bar{r}^n) - \gamma)m^n - \Delta t\beta(\bar{r}^n)m^n, \\ p^{n+1} &= p^n + \Delta t(\alpha'(\bar{r}^n) - \gamma')p^n + \Delta t\beta(\bar{r}^n)m^n - \Delta t\beta'(\bar{r}^n)p^n, \\ a_j^{n+1} &= a_j^n - \frac{\Delta t}{\Delta r} \left((V_{j+1/2}^n)^+ a_j^n - (V_{j+1/2}^n)^- a_{j+1}^n - (V_{j-1/2}^n)^+ a_{j-1}^n + (V_{j-1/2}^n)^- a_j^n \right) - \Delta t\gamma'' a_j^n, \quad j \in \{1, \dots, J\}, \\ V_{1/2}^n a_0^n &= \beta'(\bar{r}^n)p^n. \end{aligned}$$

Here above, for any real number V , $(V)^+$ and $(V)^-$ stand for the positive and negative parts of V : $(V)^+ = \max(V, 0)$ and $(V)^- = \max(-V, 0)$.

In this scheme, both integrals involved in the computation of \bar{r}^n and the $V_{j+1/2, j \in \{0, \dots, J\}}^n$ are approximated via a centered rectangle formula (thus considering that the numerical approximation of a is piecewise constant in radius). We here decide to smooth out the velocity field by replacing the discontinuous one with the following Lipschitz-continuous one

$$V(t, r) = \frac{k}{S(t)} \mathbb{1}_{[r_*, r_c - \epsilon)}(r) - \frac{r - r_c}{\epsilon} \frac{k}{S(t)} \mathbb{1}_{[r_c - \epsilon, r_c)}(r),$$

where $\epsilon > 0$ is a small parameter, which will be equal to $\epsilon = 0.005r_c$ in the simulations.

Note that, in the case of a discontinuous velocity, such as (6), we would have used instead an upwind typed scheme, that would write (see [5, 6, 9]),

$$a_j^{n+1} = a_j^n - \frac{\Delta t}{\Delta r} \left((V_j^n)^+ a_j^n - (V_{j+1}^n)^- a_{j+1}^n - (V_{j-1}^n)^+ a_{j-1}^n + (V_j^n)^- a_j^n \right) - \Delta t \gamma'' a_j^n, \quad j \in \{1, \dots, J\}.$$

We refer the reader to [9] for further details on the pros and cons of several schemes for transport with discontinuous velocities.

Stability analysis: That the numerical unknowns remain non negative, as required by the modeling, imposes constraints on the time step.

Let us consider first the ODE part of the system. We are interested in situations where the parameters satisfy

$$\alpha - \gamma - \beta(r) < 0, \quad \alpha' - \gamma' - \beta'(r) < 0 \quad \forall r \in [r_*, r_c].$$

Therefore, we expect the mesenchymal cells to decrease in time as well as the preadipocytes.

For the mesenchymal cells, the discrete relation casts as

$$m^{n+1} = (1 + \Delta t(\alpha - \gamma - \beta(\bar{r}^n))) m^n$$

Thus m^{n+1} remains non negative (if m^n is) as far as $1 + \Delta t(\alpha - \gamma - \beta(\bar{r}^n)) \geq 0$. A sufficient condition to satisfy this is that $\Delta t|\alpha - \gamma - \beta(r)| \leq 1$ for any r , thus the condition we keep is

$$\Delta t \leq \frac{1}{\max_{r \in [r_*, r_c]} |\alpha - \gamma - \beta(r)|}.$$

In the same way we derive the condition for the preadipocytes equation. In the worst situation, m vanishes and the population of preadipocytes decreases with respect to time. Thus, p^{n+1} remains non negative provided

$$\Delta t < \frac{1}{\max_{r \in [r_*, r_c]} |\alpha' - \gamma' - \beta'(r)|}.$$

Now let us consider the PDE in size space for the adipocytes. The upwind scheme is stable (in the linear case where the velocity field is given, see [5]) if the following Courant-Friedrichs-Lewy condition is satisfied:

$$\left| \frac{V^n \Delta t}{\Delta r} \right| \leq 1 \quad \forall n,$$

where

$$V^n = \max_{j \in \{1, \dots, J\}} V_j^n.$$

Therefore, at each iteration the time step is updated in order to fulfill all three conditions identified so far.

5.2. Simulations

The parameters used in the simulations are given in Table 2, according to unpublished experimental data from C3M. A fit was performed with these data in order to calibrate the parameters; a larger number of available data will be necessary to improve this calibration.

Value	Unit	Parameter or Indications
$\alpha = 0.1515$	1/day	proliferation rate for mesenchymal cells
$\alpha' = 0.0129$	1/day	proliferation rate for preadipocytes
$\beta(\bar{r}) = 0.0030 + \frac{0.1992}{1+e^{\frac{0.8550-\bar{r}}{0.0162}}}$	1/day	differentiation rate of mesenchymal cells in preadipocytes (\bar{r} normalized, $\bar{r} \times 10$ is in microns)
$\beta'(\bar{r}) = 0.06043 - \frac{0.05965}{1+e^{\frac{\bar{r}-1.1125}{-0.3640}}}$	1/day	differentiation rate of preadipocytes in adipocytes (\bar{r} normalized, $\bar{r} \times 10$ is in microns)
$\gamma = 1.5 \cdot 10^{-3}$	1/day	mortality rate for mesenchymal cells
$\gamma' = 1 \cdot 10^{-5}$	1/day	mortality rate for preadipocytes
$\gamma'' = 1.653 \cdot 10^{-6}$	1/day	mortality rate for adipocytes
$\bar{k} = 3.2875 \cdot 10^{-9}$	mol/cell/day	available food per adipocytes with $k = \bar{k} \times \# \text{adipocytes}$
$r_m = 7.5$	μm	mesenchymal cells radius
$r_* = 7.5$	μm	pre-adipocytes radius
$r_c = 50.64$	μm	maximal (critical) adipocytes radius

TABLE 2. Values for parameters and variables used in the simulations.

5.2.1. Large time behavior of the solutions to the model

The initial condition is defined as follows:

$$\begin{aligned}
 m_0 &= 2.6793 \cdot 10^5 && \text{[number of cells]} \\
 p_0 &= 7.6797 \cdot 10^3 && \text{[number of cells]} \\
 a_0(r) &= \frac{0.0311}{\sqrt{2\pi\theta}} \exp\left(-\frac{r^2}{2\theta}\right) 10^8, \text{ with } \theta = 1.003 && \text{[number of cells}/\mu\text{m]}
 \end{aligned}$$

In this initial configuration, the adipocytes have a small radius. We study the behavior of the solution in a large time scale, namely at the scale of a year ($t \in (0, 350)$ days).

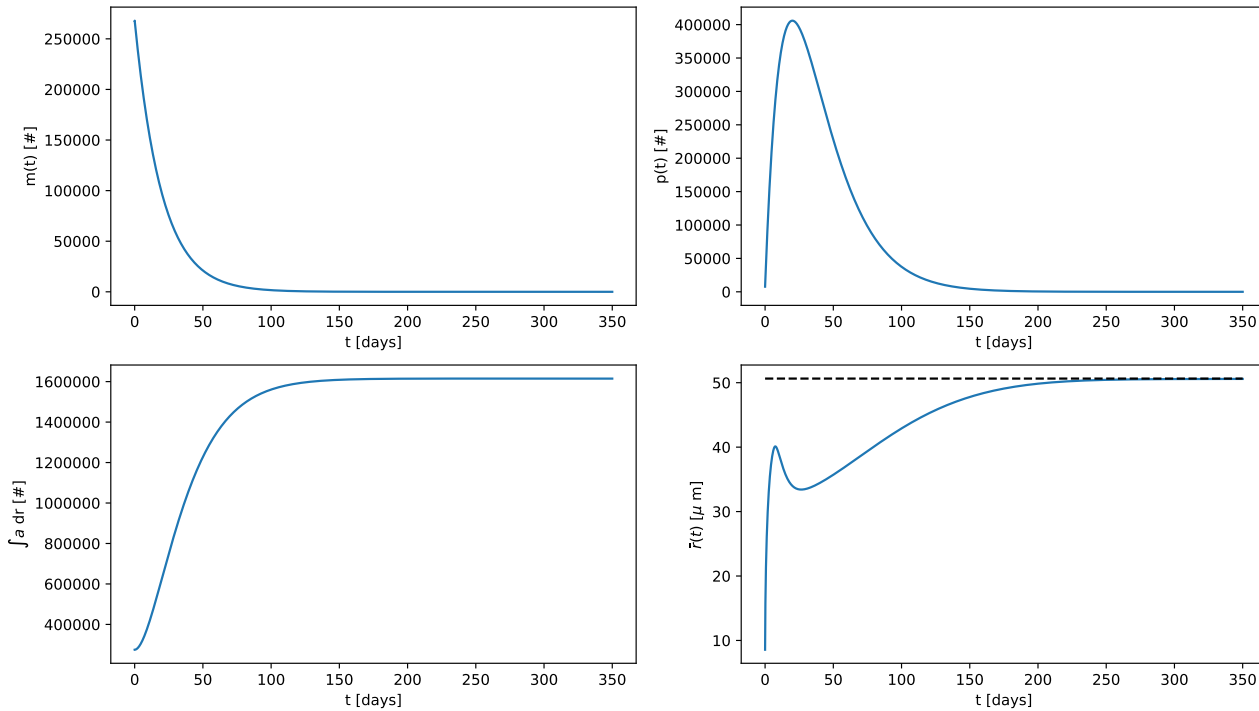


FIGURE 3. Trend of the number of cells with respect to time: mesenchymal cells (*top left*), preadipocytes (*top right*), total number of adipocytes (*bottom left*); behavior of the mean radius of adipocytes (*bottom right*).

Figure 3 shows the solution to the system of equations. Since we imposed that the proliferation rate is smaller than the sum of the differentiation and of the death rates, either the mesenchymal cells or the preadipocytes tend to zero for large time. At the beginning (first 40 days) the number of preadipocytes increases. This is due to the differentiation of the mesenchymal cells into preadipocytes. The number of adipocytes increases in time. Since we have set a very small death rate for the adipocytes ($\gamma'' \sim 10^{-6}$), the population reaches a plateau and the death of the adipocytes is not sensitive on this time scale of observation. We observe that the mean radius of the adipocytes grows rapidly at the beginning (first 10 days). Then, there is a drop due to the differentiation of preadipocytes into adipocytes: indeed, this process produces a large number of new adipocytes which have a radius equal to r_* . Next, these small adipocytes grow until their radius reaches the critical value r_c . The adipocytes growth can equally be observed in Figure 4. Initially, the adipocytes are small and they are subjected to a strong growth rate, since the growth rate is proportional to the inverse of the total surface of adipocytes. When the cells grow, the rate decreases because of an increasing of the surface of adipocytes. Figure 5 shows the distribution of adipocytes at the last time step. We observe the accumulation of the adipocytes population to the critical radius and the formation of the Dirac mass, according to the theoretical results.

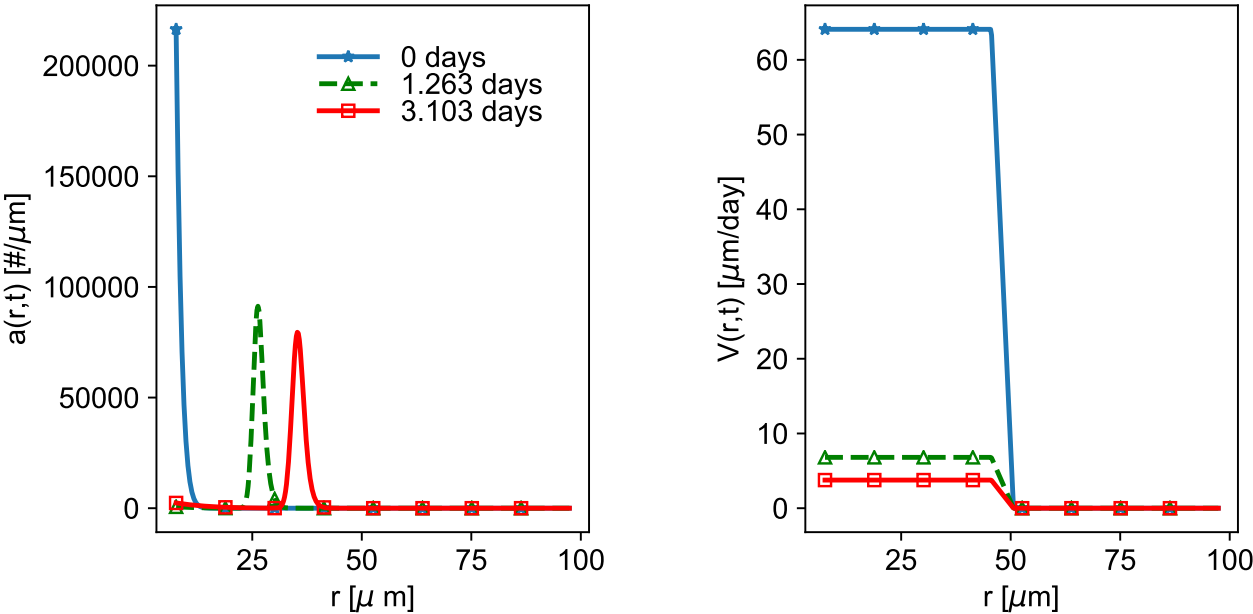


FIGURE 4. Adipocytes distribution (*left*) and growth rate (*right*) with respect to the radius at three different time steps.

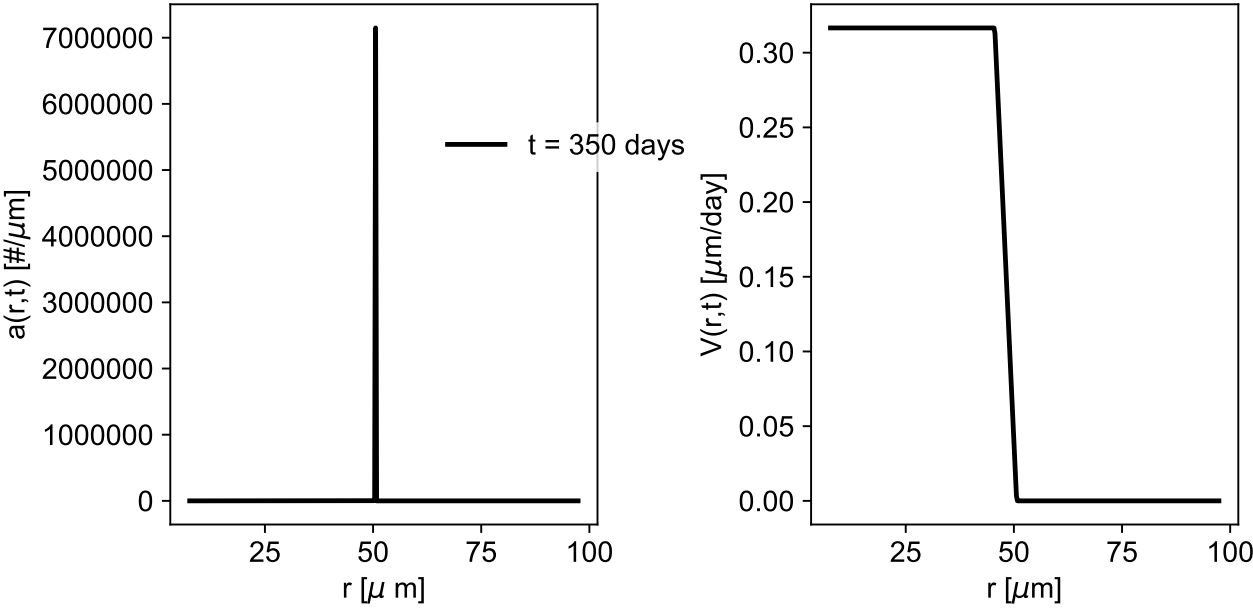


FIGURE 5. Adipocytes distribution (*left*) and growth rate (*right*) with respect to the radius at the last time step.

5.2.2. Differentiation rates

We now observe the behavior of the proliferations rates $\beta(\bar{r}(t))$ and $\beta'(\bar{r}(t))$. Figure 6 shows the dependency of the two functions with respect to the radius and to time (with parameters as given in Table 2). Since the mean radius increases rapidly, also the differentiation rates reach rapidly the maximum value.

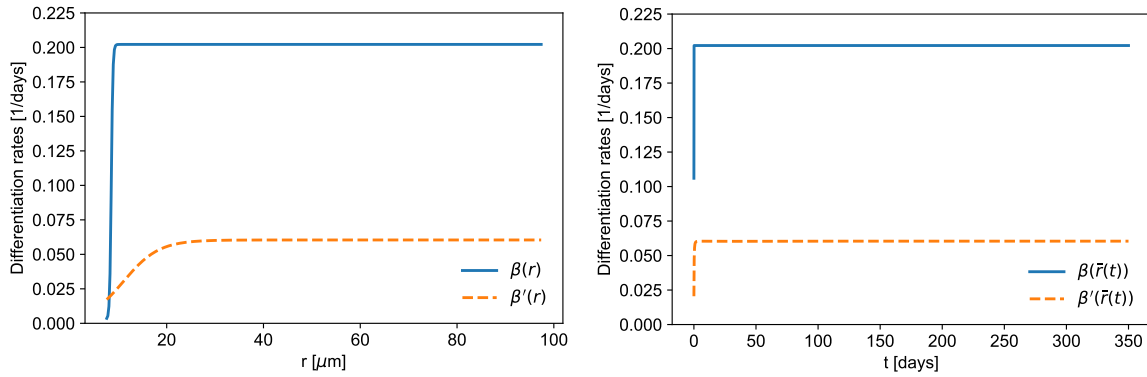


FIGURE 6. Differentiation rates of the mesenchymal cells (blue continuous line) and the preadipocytes (orange dotted line) with respect to the radius (*left*) and to time (*right*).

The qualitative behaviour does not change significantly when working with constant differentiation rates (see Figure 7). It likely means that the quantities of interest remain in the low or high regions of the sigmoid in this example.

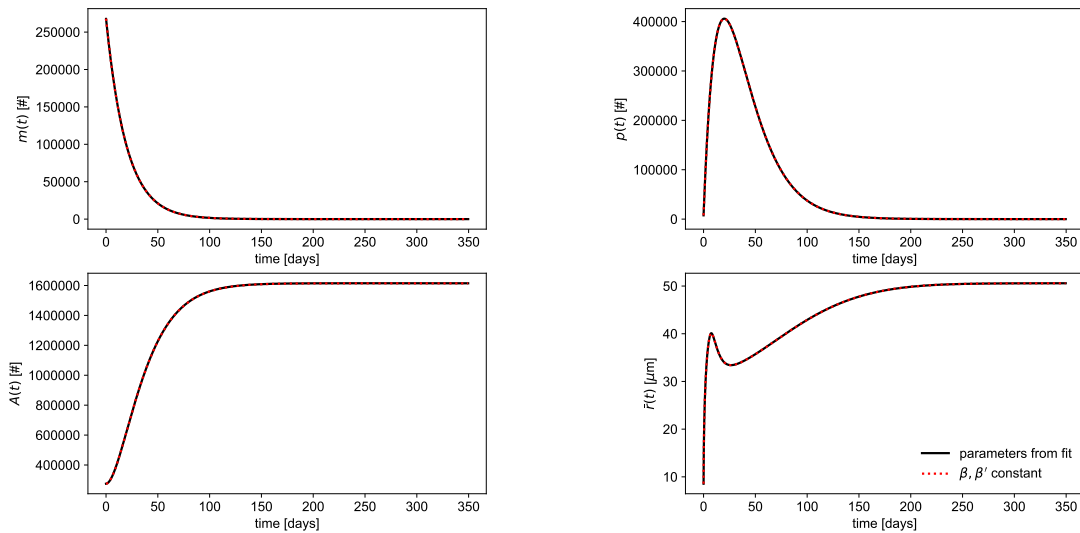


FIGURE 7. Comparison between the cases when β and β' are sigmoid functions (black line) and constant (red dotted line).

However, changing the parameters of the the sigmoid functions β and β' can lead to different behaviors of the solutions. We consider three cases, detailed in Table 3: we fix the slope of the sigmoid functions and we make the inflection points vary. Figure 8 shows the comparison of the populations dynamics in the different cases. The larger the inflection point of β' , the more preadipocyte are generated, and therefore differentiate. In fact, since the differentiation rate is slower, they have time to duplicate. However, the dynamics of the adipocytes and of the mean radius in Figure 8 suggest that the parameters considered in Table 2 are in good agreement with the experimental data.

	$r_{ip,\beta}$	$r_{ip,\beta'}$
case 1	$0.5r_c$	$0.5r_c$
case 2	$0.5r_c$	r_c
case 3	$0.5r_c$	$0.7r_c$

TABLE 3. Inflection points relative to β and β' in the different cases.

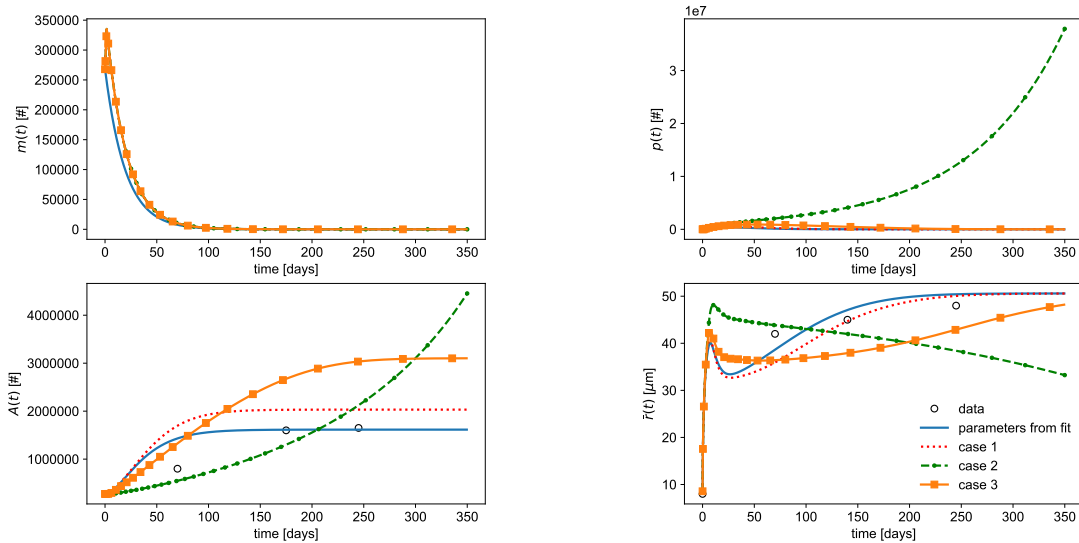


FIGURE 8. Dynamics of the different cells (mesenchymal cells on the top left; preadipocytes on the top right; adipocytes on the bottom left) and of the mean radius of the adipocytes (bottom right) according to different shapes of the differentiation rates. The blue line refers to the parameters set in Table 2 and the black circles to the experimental data.

5.2.3. Comparison with experimental data

We now compare the models with the experimental data. We test the model structured in size (1) (referred to as 0D), and the models structured in both size and space, which will be detailed in the next sections: we refer to these models as 1D and 2D, depending on the space dimension used in the simulations. We observe in Figure 9 that the solutions to the 0D, the 1D and the 2D models have similar behavior. Since the 0D model has been calibrated with the data, it is in good agreement with the experimental data.

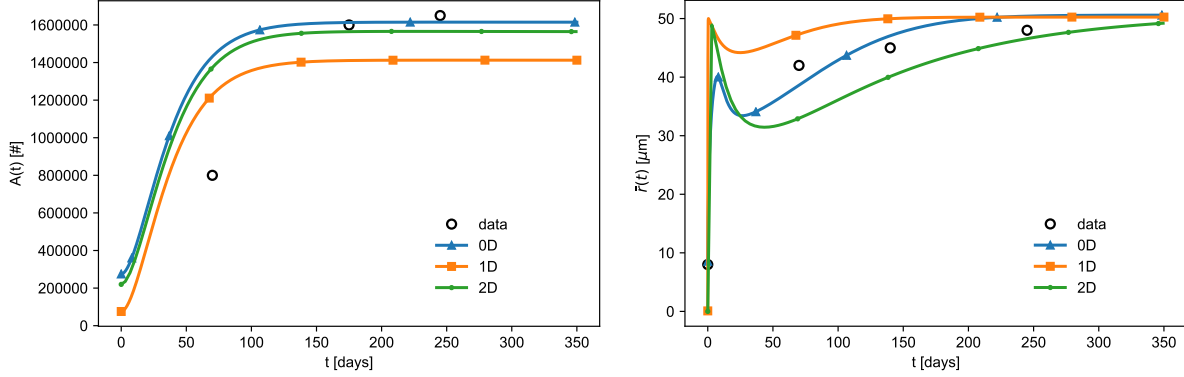


FIGURE 9. Comparison of the models with the experimental data: adipocytes number (*left*) and mean radius (*right*).

6. EXTENSION TO A SPATIAL MODEL

6.1. Reinterpretation of the unknowns

We are now going to extend the previous model by incorporating a spatial dependence intended to describe inhomogeneities and displacement of the adipose tissue, following some ideas of mixture theory, see [1, 3, 8]. The functions $(t, x) \mapsto m(t, x)$, $(t, x) \mapsto p(t, x)$ now depend also on the space variable $x \in \Omega \subset \mathbb{R}^n$ ($n = 1$ or 2 , and Ω is a bounded domain), and they are defined on $[0, \infty) \times \Omega$ with values in $[0, \infty)$. For the adipocytes, $(t, x, r) \mapsto a(t, x, r)$ is a function defined on $[0, \infty) \times \Omega \times [r_*, +\infty)$ with values in $[0, \infty)$. We also introduce a new function $(t, x) \mapsto s(t, x)$ which is the volume fraction of the surrounding material (tissue) that is carrying the cells. The motion of all these species is driven by a velocity field $(t, x) \mapsto u(t, x)$.

In order to derive the model, let us go back to the mass balance relations. Given $r_2 > r_1 \geq r_*$, the integral

$$\frac{4\pi}{3} \int_0 \int_{r_1}^{r_2} a(t, x, r) r^3 dr dx,$$

gives the volume occupied in O at time t by the adipocytes with a radius $r \in (r_1, r_2)$. Accordingly,

$$\frac{4\pi}{3} \int_{r_*}^{\infty} a(t, x, r) r^3 dr$$

defines the volume fraction of the adipocytes, and the total volume of functional adipocytes at time t is given by

$$\mathbb{V}(t) = \frac{4}{3} \pi \int_{\Omega} \int_{r_*}^{\infty} s^3 a(t, x, s) ds dx.$$

Schematically, we can split the volume of an adipocyte with radius $r \geq r_*$ into two parts, see Fig. 10: the center, with radius r_* , is mainly made of water (volumetric mass density ρ_w), like the pre-adipocytes and mesenchymal cells, while the outer domain is made of lipids (volumetric mass density ρ_l). Therefore, the mass of such an adipocyte reads

$$\frac{4\pi}{3} (\rho_l (r^3 - r_*^3) + \rho_w r_*^3) = \frac{4\pi}{3} \rho_a(r) r^3$$

with

$$\rho_a(r) = \frac{\rho_l (r^3 - r_*^3) + \rho_w r_*^3}{r^3} \quad \text{for } r \geq r_*.$$

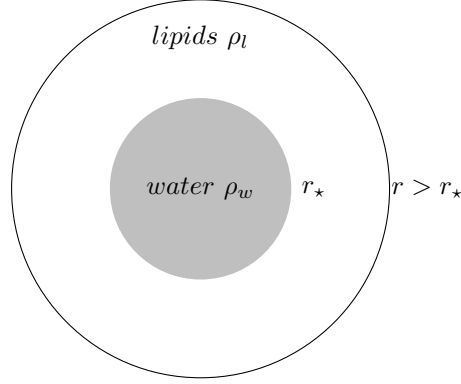


FIGURE 10. Growing adipocyte.

Accordingly, the mass density of the adipocytes is given by

$$M_a(t, x) = \frac{4\pi}{3} \int_{r_*}^{\infty} \rho_a(r) a(t, x, r) r^3 dr,$$

and the total mass of adipocytes reads $\int_{\Omega} M_a(t, x) dx$. The evolution of the mass density obeys

$$\partial_t M_a(t, x) = -\frac{4\pi}{3} \int_{r_*}^{\infty} \gamma'' \rho_a(r) a(t, x, r) r^3 dr + \frac{4\pi r_*^3}{3} \rho_w \beta'(\bar{r}(t, x)) p(t, x) + 4\pi \int_{r_*}^{\infty} \rho_l V a(t, x, r) r^2 dr.$$

The last two terms describe two mechanisms of gain of mass: the transformation of pre-adipocytes into adipocytes with radius r_* and volumetric mass density ρ_w and the input of lipids from the surface of the existing adipocytes.

Similarly, the volume fractions of mesenchymal cells and pre-adipocytes are given by

- $\frac{4\pi}{3} r_m^3 m(t, x)$ for the mesenchymal cells,
- $\frac{4\pi}{3} r_*^3 p(t, x)$ for the preadipocytes,

respectively, with r_m and r_* the typical radius of these cells. According to the biological data, we will use from now on that $r_m = r_*$.

Given $O \subset \Omega$, the integrals $\int_O \frac{4\pi}{3} r_*^3 m(t, x) dx$ and $\int_O \frac{4\pi}{3} r_*^3 p(t, x) dx$ gives the volume occupied in O at time t by the mesenchymal cells and the preadipocytes, respectively.

The mass of each species is transported by a velocity field $(t, x) \in [0, \infty) \times \Omega \mapsto u(t, x) \in \mathbb{R}^n$, which amounts to say

$$\begin{cases} \frac{4\pi r_*^3}{3} \rho_w \left(\frac{\partial m}{\partial t} + \operatorname{div}_x(mu) - (\alpha - \gamma - \beta)m \right) = 0, \\ \frac{4\pi r_*^3}{3} \rho_w \left(\frac{\partial p}{\partial t} + \operatorname{div}_x(pu) - (\alpha' - \gamma' - \beta')p - \beta m \right) = 0, \\ \frac{\partial s}{\partial t} + \operatorname{div}_x(su) = 0. \end{cases} \quad (30)$$

For the adipocytes, we get

$$\partial_t(\rho_a r^3 a) + \nabla_x \cdot (\rho_a r^3 ua) + \rho_a r^3 \partial_r (Va) = -\gamma'' \rho_a r^3 a$$

which can also be written in the conservative form

$$\partial_t(\rho_a r^3 a) + \nabla_x \cdot (\rho_a r^3 ua) + \partial_r (\rho_a r^3 Va) - 3\rho_l r^2 (Va) = -\gamma'' \rho_a r^3 a \quad (31)$$

In fact, we can get rid of the densities in all these equations, and (31) can be simplified as:

$$\partial_t a + \nabla_x \cdot (ua) + \partial_r (Va) = -\gamma'' a. \quad (32)$$

Beyond the transport by the velocity u , the modeling also uses a pressure field, hereafter denoted $(t, x) \mapsto q(t, x)$; we shall assume that the parameters β and β' are now functions of both \bar{r} and this quantity q . It incorporates another source of space inhomogeneities. We assume that β, β' are non decreasing with respect to q . The pressure acts as a mechanical constraint that limits the expansion of the adipocytes: the weaker the pressure, the easier the transformation of mesenchymal cells and pre-adipocytes to pre-adipocytes and adipocytes, respectively.

Let us now discuss the equations for the pair (u, q) . The following constraint on the volume fractions holds, (using that the radius of pre-adipocytes and of mesenchymal cells coincides with the radius r_* of the smallest adipocytes)

$$s(t, x) + \frac{4\pi}{3} \left(r_*^3 m(t, x) + r_*^3 p(t, x) + \int_{r_*}^{+\infty} r^3 a(t, x, r) dr \right) = 1, \quad (33)$$

for a. e. $x \in \Omega, t \geq 0$. Therefore, adding the equations in (30) and (32), we find

$$\operatorname{div}_x u = \frac{4\pi}{3} \left(r_*^3 (\alpha - \gamma) m + r_*^3 (\alpha' - \gamma' - \beta') p - \int_{r_*}^{\infty} r^3 \partial_r (Va) dr \right).$$

Using the same boundary condition as (3), we obtain

$$\operatorname{div}_x u = \frac{4\pi}{3} \left(r_*^3 (\alpha - \gamma) m + r_*^3 (\alpha' - \gamma') p + 3 \int_{r_*}^{\infty} r^2 Va dr \right). \quad (34)$$

Again, we observe that the last term can be integrated by parts to make two contributions appear, the former from the passage of pre-adipocytes to adipocytes with size r_* , the latter due to surface fluxes of lipids. This constraint is related to the pressure q , which may be seen as the corresponding Lagrange multiplier.

Next, we use Darcy's equation:

$$u(t, x) = -K(x) \nabla_x q(t, x) \text{ in } \Omega, \quad (35)$$

which have different frames of application [4, 11]. In (35), $x \mapsto K(x)$ takes values in the set of symmetric positive matrices. With (35) we are directly led to an equation for q , by using equation (34)

$$\begin{aligned} -\operatorname{div}_x (K(x) \nabla_x q) &= \operatorname{div}_x u \\ &= \frac{4\pi}{3} \left(r_*^3 (\alpha - \gamma) m + r_*^3 (\alpha' - \gamma') p + 3 \int_{r_*}^{\infty} r^2 Va dr \right). \end{aligned}$$

We complement the whole system with initial conditions:

$$\begin{aligned} m(0, x) &= m_0(x), p(0, x) = p_0(x), s(0, x) = s_0(x), a(0, x, r) = a_0(x, r), \\ u(0, x) &= u_0(x) \end{aligned}$$

satisfying constraint (33).

Finally, we need to impose boundary conditions. For $r = r_*$, we make use of the same birth condition as in the homogeneous case

$$V(t, r_*) a(t, x, r_*) = \beta'(\bar{r}(t, x), q(t, x)) p(t, x).$$

On $\partial\Omega$, we shall find boundary conditions. For example, we can use

- for cells, the no-incoming-flux condition:

$$\text{if } u \cdot n < 0, \text{ then } a = p = m = 0 \text{ and } s = 1$$

where n stands for the unit outward normal vector on $\partial\Omega$, we also set

$$q = 0 \text{ on } \partial\Omega.$$

- or the wall conditions.

These boundary conditions have to be compatible with condition (34).

6.2. Description of the numerical discretization

In order to discretize the system of equations, we apply the finite volume method. First, we find the spatial velocity u solving the Darcy's law. We formulate the Darcy's equation as a Laplace problem:

$$\begin{cases} -\operatorname{div}(K\nabla q) = \operatorname{div}u, & \text{in } \Omega, \\ q = 0, & \text{on } \partial\Omega, \end{cases} \quad (36)$$

From (36) we compute the pressure q . Then, we find the velocity \mathbf{u} thanks to

$$u = -K\nabla q, \quad \text{in } \Omega.$$

Applying the finite volume method, we obtain the following discretization on each element \mathcal{K}_i of the domain.

$$\begin{aligned} -\int_{\mathcal{K}_i} \operatorname{div}(K\nabla q) dx &= \int_{\mathcal{K}_i} \operatorname{div}(u) dx \\ -[K\nabla q \cdot n]_{\partial\mathcal{K}_i} &= \int_{\mathcal{K}_i} \operatorname{div}(u) dx \end{aligned}$$

Finally, we apply an explicit upwind scheme in order to solve the system of hyperbolic equations. Regarding the adipocytes, we use a “directional” splitting and solve the transport equation either in space or with respect to the radius dimension applying the finite volume upwind scheme.

6.3. Numerical simulations for the spatial case

In one dimension, we consider an interval $(0, L)$ where $L = 1$ cm, therefore $x \in \Omega = (0, 0.01)$. We discretize the interval in $J = 300$ subintervals with a homogeneous spatial step Δx . Moreover, we have to consider the “radius” dimension of the adipocytes. To approximate their growth, we consider the radius of the adipocytes r to be in the interval $I_r = (r_*, R)$, and we set $R = 90\mu\text{m}$. We divide I_r into 100 homogeneous intervals of size Δr . Then, we solve the problem that has one dimension with respect to the mesenchymal cells m and the preadipocytes p and two dimensions with respect to the adipocytes a .

Parameters setting and initial conditions

The parameters used for the simulations are the ones introduced in Table 2. Regarding the initial condition, we consider the three populations to be distributed as gaussians centered in

different points of Ω with various standard deviations (with respect to space and radius), namely

$$\begin{aligned} m_0(x) &= \frac{m_0}{\sqrt{2\theta^2 L^2 \pi}} \exp\left(-\frac{(x-x_m)^2}{2\theta^2 L^2}\right), \\ p_0(x) &= \frac{p_0}{\sqrt{2\theta^2 L^2 \pi}} \exp\left(-\frac{(x-x_p)^2}{2\theta^2 L^2}\right), \\ a_0(x, r) &= \left(\bar{a}_0 + \frac{a_0}{\sqrt{2\pi\theta_r} \sqrt{\theta_a^2 L^2 \pi}} \exp\left(-\frac{r^2}{2\theta_r}\right) \exp\left(-\frac{(x-x_a)^2}{\theta_a^2 L^2}\right)\right) \mathbf{1}_{r < r_c}. \end{aligned}$$

For the numerical simulations, we take the following values for the standard variations : $\theta = 0.1$, $\theta_r = 0.1$, $\theta_a = 0.8$.

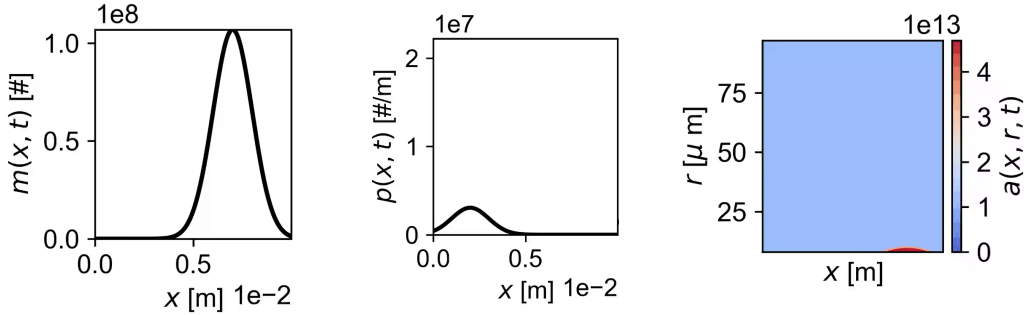


FIGURE 11. Initial conditions for m (left), p (center) and a (right) relative to the 1D spatial model. The figure on the right represents the distribution of a in each point of the space x and with a radius r .

Figure 11 shows the initial conditions of the three unknowns. At the beginning we consider the highest number of adipocytes to have the minimal radius r_* . However, since the growth rate is proportional to the inverse of the surface of adipocytes in each spatial point, we consider minimum number of cells \bar{a}_0 in each spatial point.

Simulations

We study the behavior of the populations and of the mean radius first looking at a small time scale. In particular, we focus on the growth of the initial adipocytes. Figure 12 shows the adipocyte dynamic in the first day. We observe a slow growth of cells at the center of the initial gaussian, where the total surface of the cells is the highest. If we move from this point, the total surface of the cells decreases and consequently the radius of the cells increases faster. In Figure 13 we observe the global growth of adipocytes at different time steps. Like with the space homogeneous equations, we observe a high growth rate at the beginning, leading to a fast growth of the adipocytes at the initial configuration.

Since the spatial velocity is very small, we do not observe a displacement of the different cells in the interval. The spatial dependency indeed introduces two different timescales relative to the growth of adipocytes and to the spatial displacement.

We observe on numerical simulations, see Fig.13, that dealing with the space dependent framework favors the apparition of bimodal size-distributions, that have been recorded in experiments, see [17, 18]. We were unable to reproduce such bimodal shape with the space homogeneous model. It is likely that such distributions correspond only to transient states of the model; nevertheless they can be relevant on the time scale of observation. Going further in this direction requires a better knowledge of the parameters of the model and deserves a thorough investigation.

7. CONCLUSION

This work aims at setting up the basis of a multi-species model for adipose tissue growth, with the aim of improving our understanding of obesity. Our model is based on detailed behaviors and interactions of adipose tissue cells. It accounts for the adipocyte maturation, starting from mesenchymal cells differentiating into pre-adipocytes, which in turn differentiate into adipocytes whose sizes grow with food supply. The core of our model is the coupled regulation of cell differentiation and proliferation using phenomenological laws with sigmoid shapes that depend on the mean size of adipocytes.

The model in its non-spatial version is able to reproduce with reasonable precision experimental data after a fitting process, indicating that the main biological phenomena are probably accounted for in our model hypotheses. The time dynamics of the adipocyte radii exhibits an interesting early overshoot that cannot be seen in the data because of its sampling. The overshoot is easily explained by the model dynamics and its existence could be investigated in future experimental work. A shift in early adipocyte numbers is also observed, probably because of the difficult choice of an initial condition in the absence of a more detailed set of data.

The spatial model also keeps a reasonable agreement with the data, at least in order of magnitude and allows to exhibit a well known behavior for adipocyte distribution: a bimodal distribution of adipocytes in space [17,18]. This last result can be seen as a first step for validation of our model and makes it very promising. The fact that we do not observe spatial displacements of the cells needs more investigations and we can consider the mechanical properties of adipose tissues described in [13] to improve the spatial description in our model.

The next step is now to gather more complete data sets from experimental studies and to reach a proper validation. Once validated, such a model could prove invaluable to identify and quantify the biological mechanisms involved in adipose tissue growth and to understand potential dysfunctions linked to obesity.

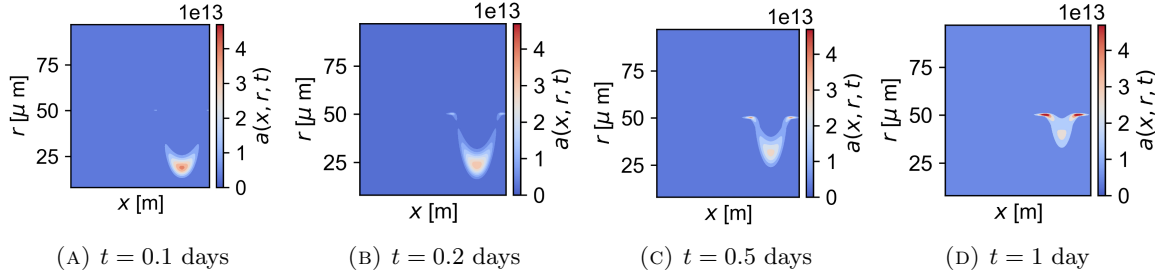


FIGURE 12. Adipocytes distribution with respect to space and radius at different time steps.

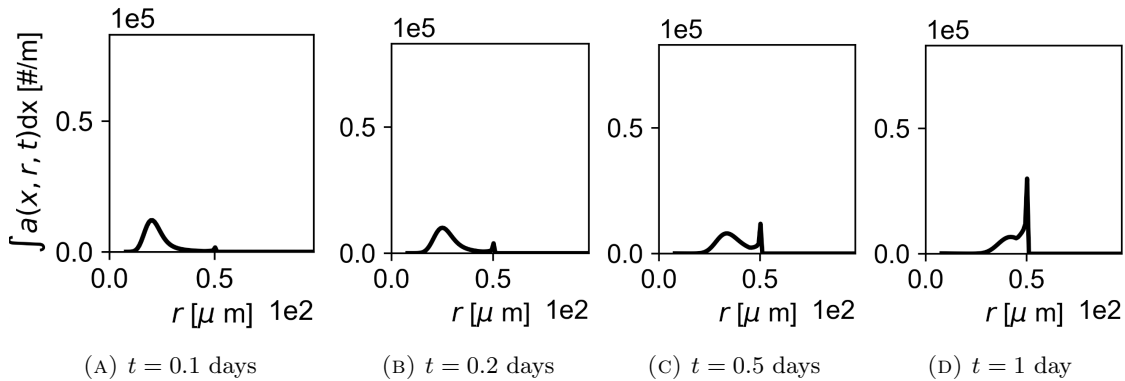


FIGURE 13. Adipocytes distribution with respect to the radius at different time steps.

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