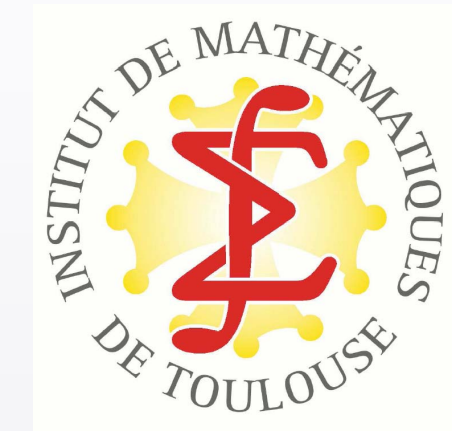


Mathematical modeling of embryo axis elongation

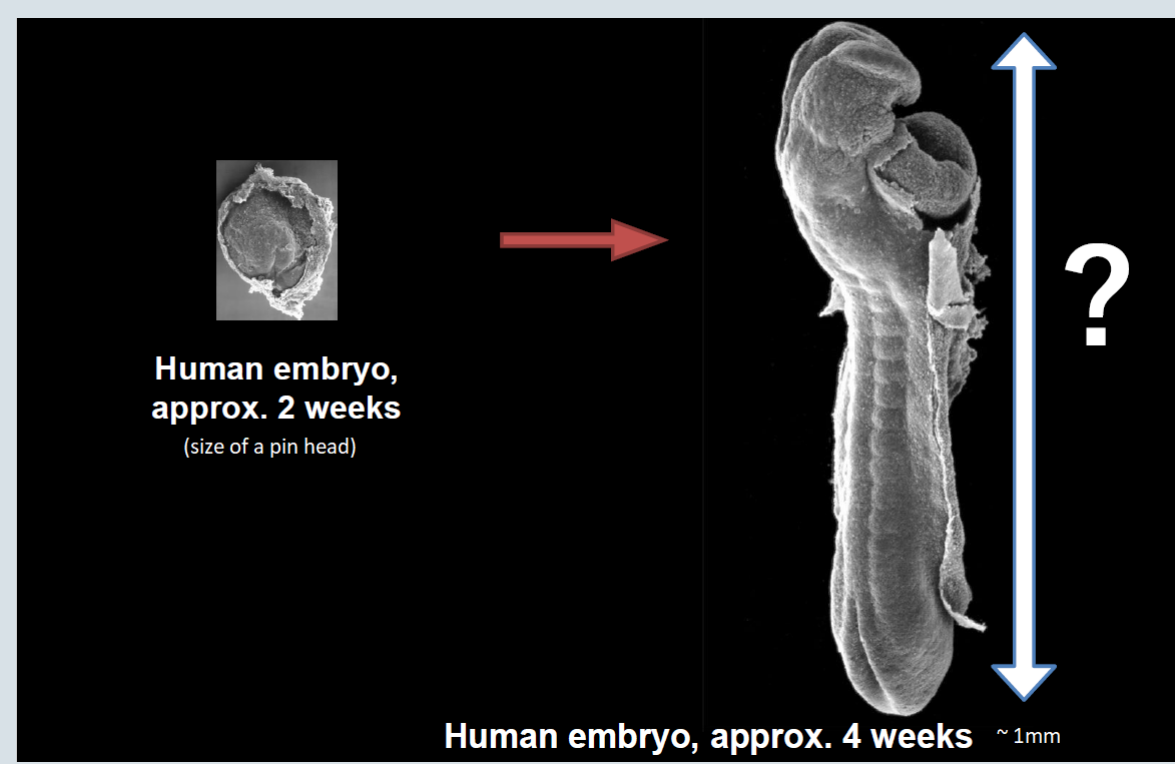
Michèle Romanos – Institut de Mathématiques de Toulouse

Supervisors: Ariane Trescases (IMT) and Bertrand Bézazéraf (CBI)



1 – INTRODUCTION TO THE BIOLOGICAL MODEL

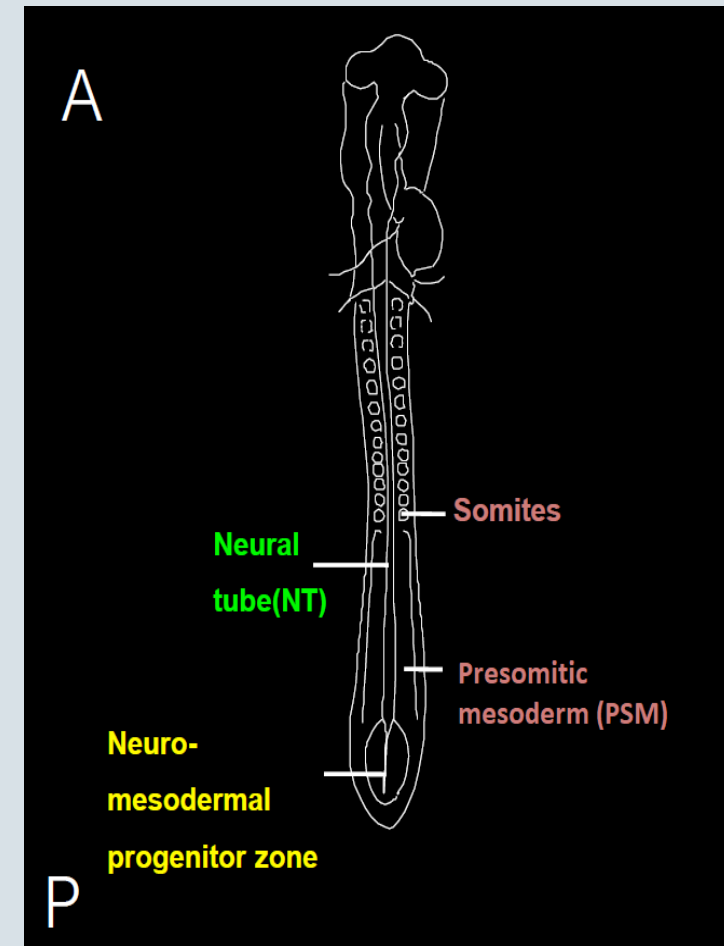
During embryonic development thousands of cells self-organize in a very precise and complex choreography to form the tissues and the future adult organs.



Human embryo development

Coordination between:

- Cellular proliferation
- Migration
- Adhesion
- Addition of new cells



Different tissues involved in bird development

How is this coordination contributing to the rise of mechanisms causing elongation?

2 – THE VISCOUS TWO SPECIES MODEL

Consider the densities n_1 and n_2 of two cell populations in each tissue. Each tissue is endowed with a viscosity coefficient β_1 and β_2 , a proliferation rate G_1 and G_2 , a mechanical pressure $p_\epsilon = \epsilon \frac{n_1+n_2}{1-(n_1+n_2)}$, and a repulsion term $q_m = \frac{m}{m-1}((1+n_1n_2)^{m-1} - 1)$, and v_1, v_2 the velocities of each tissue which follow the Brinkman law:

$$\partial_t n_1 + \nabla \cdot (n_1 v_1) + \alpha \nabla \cdot (n_1 \nabla (\Delta n_1)) = n_1 G_1(p_1), \quad (1)$$

$$\partial_t n_2 + \nabla \cdot (n_2 v_2) + \alpha \nabla \cdot (n_2 \nabla (\Delta n_2)) = n_2 G_2(p_2), \quad (2)$$

$$p_1 = p_\epsilon (n_1 + n_2) + n_2 q_m (n_1 n_2), \quad (3)$$

$$p_2 = p_\epsilon (n_1 + n_2) + n_1 q_m (n_1 n_2), \quad (4)$$

$$-\beta_1 \Delta v_1 + v_1 = -\nabla p_1 \quad (5)$$

$$-\beta_2 \Delta v_2 + v_2 = -\nabla p_2 \quad (6)$$

with α a regularizing parameter (avoid bubble effect), ϵ and m parameters of the pressure laws.

3 – THE FREE BOUNDARY PROBLEM: $\alpha \rightarrow 0, m \rightarrow \infty, \epsilon \rightarrow 0$

Objective: Computing the incompressible limit of the viscous two-species model when $\alpha \rightarrow 0, m \rightarrow \infty$, and $\epsilon \rightarrow 0$.

We formally determine this limit and find the following free-boundary problem:

$$\partial_t n_1^\infty + \nabla \cdot (n_1^\infty v_1^\infty) = n_1^\infty G_1(p_1^\infty), \quad (7)$$

$$\partial_t n_2^\infty + \nabla \cdot (n_2^\infty v_2^\infty) = n_2^\infty G_2(p_2^\infty), \quad (8)$$

$$p_1^\infty = p^\infty + n_2^\infty q^\infty, \quad (9)$$

$$p_2^\infty = p^\infty + n_1^\infty q^\infty, \quad (10)$$

$$-\beta_1 \Delta v_1^\infty + v_1^\infty = -\nabla p_1^\infty \quad (11)$$

$$-\beta_2 \Delta v_2^\infty + v_2^\infty = -\nabla p_2^\infty \quad (12)$$

Moreover we have the following relation

$$p^\infty (1 - (n_1^\infty + n_2^\infty)) = 0,$$

the segregation property at the limit: $n_1^\infty n_2^\infty = 0$ and the complementary relation:

$$(p^\infty)^2 \left(n_1^\infty \nabla \cdot v_1^\infty + n_2^\infty \nabla \cdot v_2^\infty \right) = (p^\infty)^2 \left(n_1^\infty G_1(p_1^\infty) + n_2^\infty G_2(p_2^\infty) \right)$$

We define the moving domain

$$\Omega(t) = \{x | p^\infty > 0\} = \{x | n_1^\infty + n_2^\infty = 1\} \text{ a.e.} \quad (13)$$

Finally we get the velocities of the free boundaries and the continuity condition on the interface $\Gamma(t)$

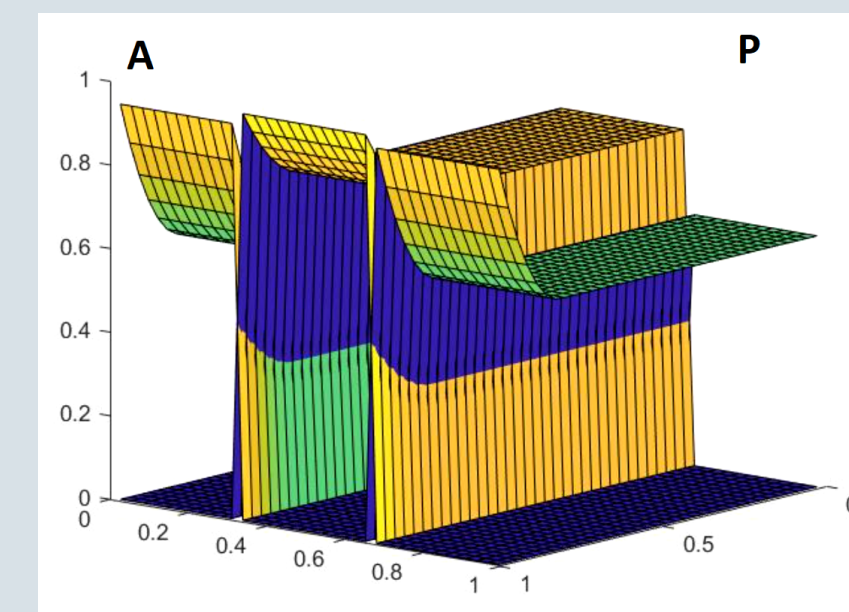
$$V_{\partial\Omega_1(t) \cap \partial\Omega(t)} = v_1^\infty \cdot \vec{\nu}, \quad V_{\partial\Omega_2(t) \cap \partial\Omega(t)} = v_2^\infty \cdot \vec{\nu}, \quad \text{and} \quad v_1^\infty \cdot \vec{\mu} = v_2^\infty \cdot \vec{\mu} \quad \text{on} \quad \Gamma(t)$$

with $\vec{\nu}$ the outward normal vector to the boundary and $\vec{\mu}$ that of the interface.

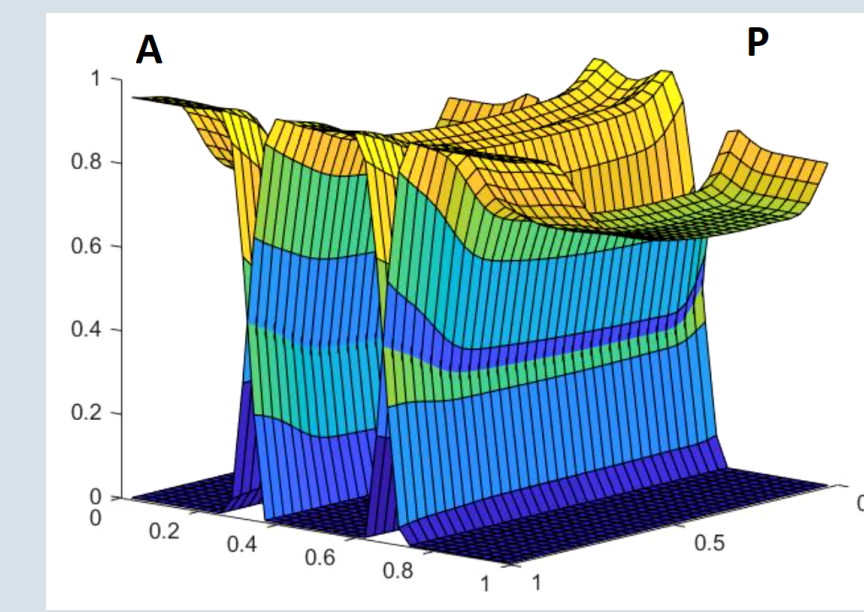
4 – NUMERICAL SIMULATIONS

We use a 2D finite volume scheme to simulate the evolution of the densities, and the flux in each tissue:

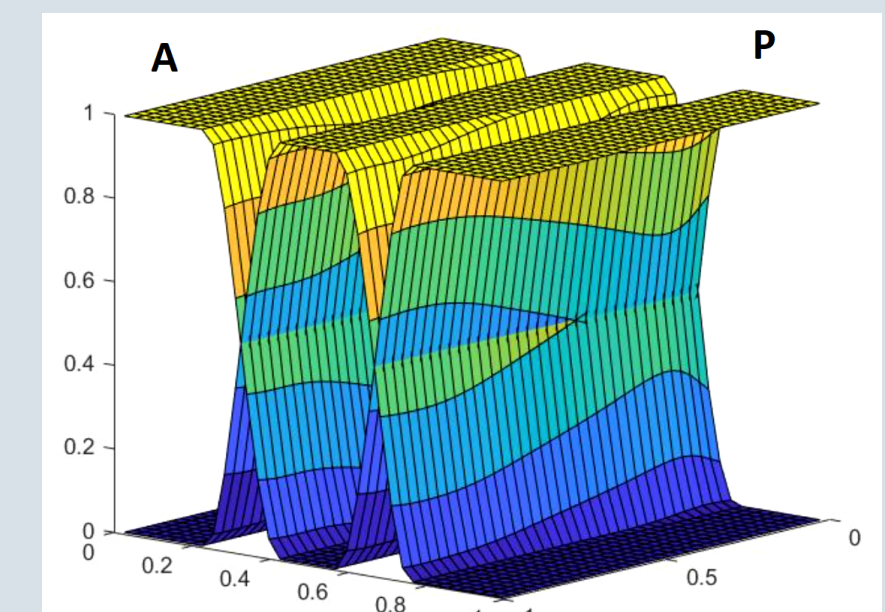
Density profile:



0h of development.

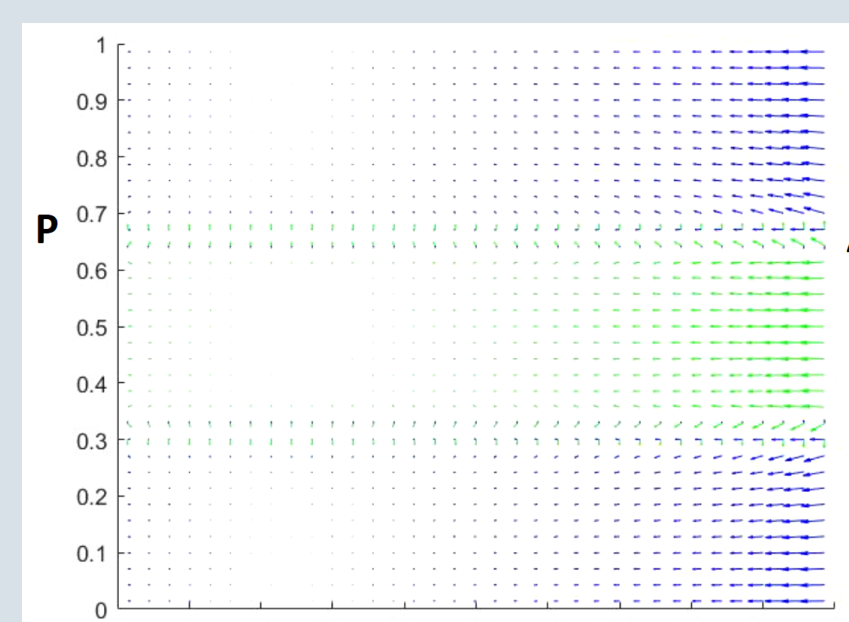


After 10min of development.

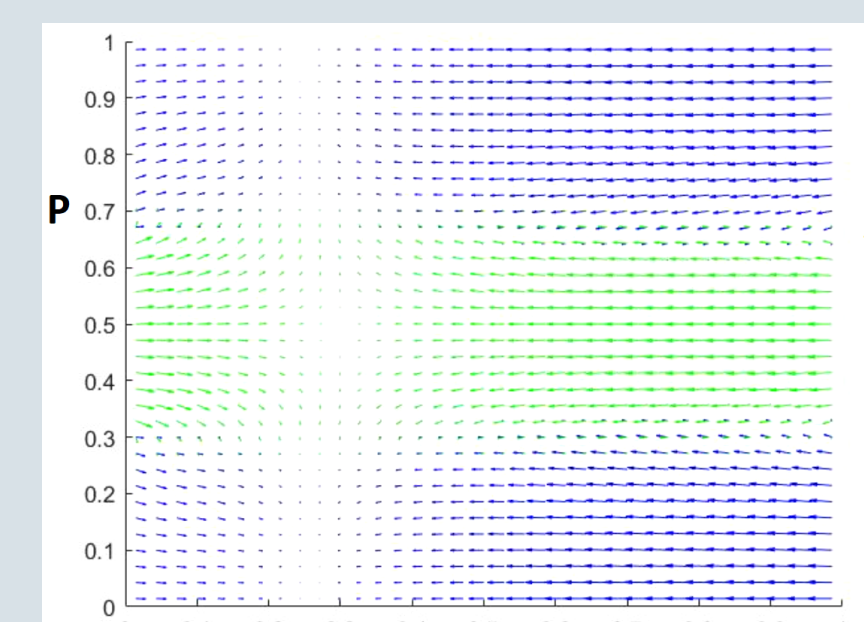


After 1h of development.

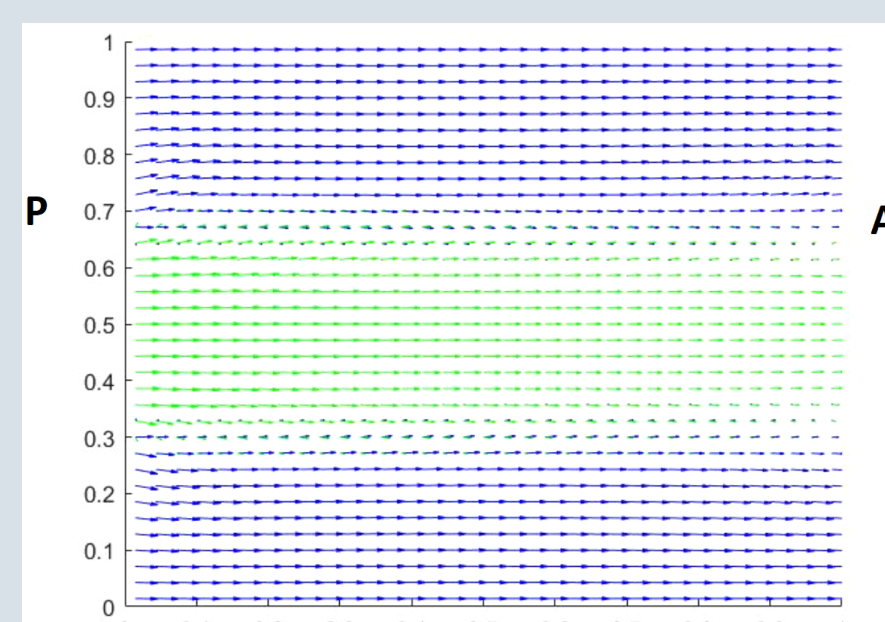
Flux profile:



0h of development.



After 10min of development.



After 1h of development.

Main challenges: Blow up of the pressure when the density is close to its maximum value, strict CFL conditions, calibrating the model parameters to fit the biological data...

5 – CONCLUSION AND PERSPECTIVES

Experimentally: Ongoing work with B. Bézazéraf

Objective: Validate the model and generate new biological hypotheses

Varying the model parameters such as: proliferation rates, viscosity coefficients, incoming flux from the progenitor zone (boundary conditions) allows us to generate new biological hypotheses and analyse:

- Sliding between the tissues
- Differential growth

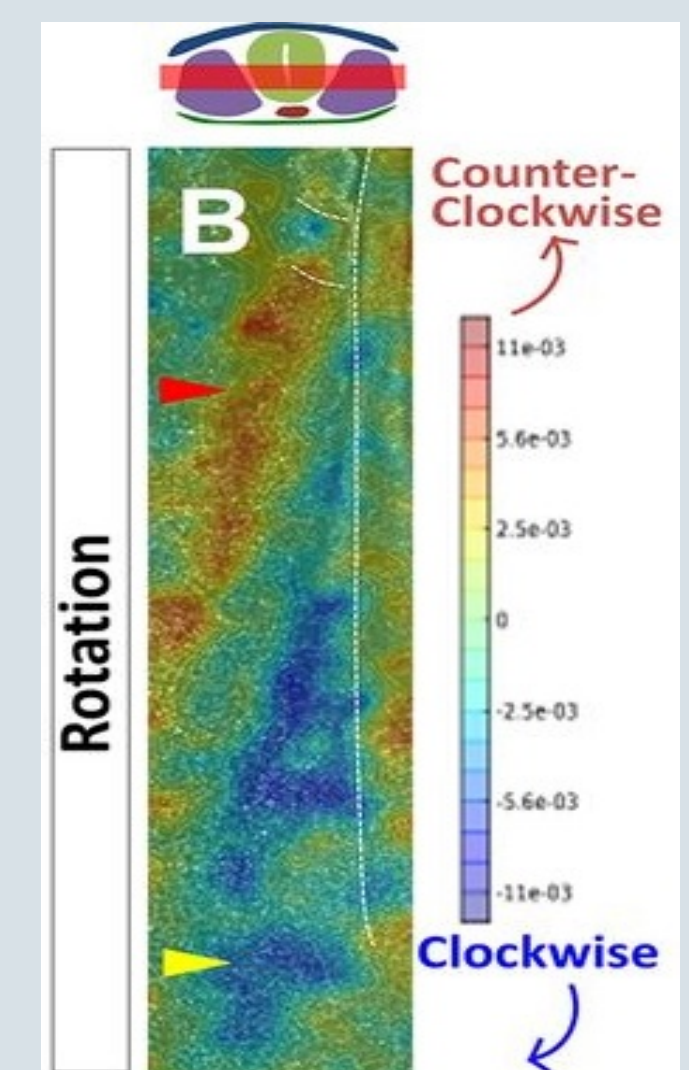
To validate the new hypotheses of the model i will harvest quail eggs and:

- Inhibit proliferation
- Control the incoming flux from the progenitor zone
- Track cells using live imaging to compare with in silico experiments

Mathematically: Ongoing work with S. Hecht, P. Degond, A. Trescases

Objective: Prove rigorously the limit to the free boundary problem - in the spirit of [4] (one species)

- **New difficulty:** two-species [1], without considering the velocity as a gradient
- **Achieved:** Well posedness of the limit system in a case test (one species, homogeneous Dirichlet boundary conditions)
- Extend previous result to more general boundary conditions, for two-species



Rotational movement of cells observed in bird embryos. [3]

6 – REFERENCES

1. T. Debiec and M. Schmidtechen *Incompressible limit for a two-species tumour model with coupling through Brinkman's law in one dimension* (2019).
2. A. Chertock, P. Degond, S. Hecht, and J-P. Vincent *Incompressible limit of a continuum model of tissue growth with segregation for two cell populations* (2018).
3. B. Bézazéraf, M. Beaupeux and M. Tchernookov *Multi-scale quantification of tissue behavior during amniote embryo axis elongation* (2017)
4. B. Perthame and N. Vauchelet *Incompressible limit of mechanical model of tumor growth with viscosity.* (2014)